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(54) **ROBOTIC GUIDE ASSEMBLY FOR USE IN
COMPUTER-AIDED SURGERY**

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2017/1602 (2013.01); **A61B 2034/2055**
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606/86 R, 87, 96, 97, 98

See application file for complete search history.

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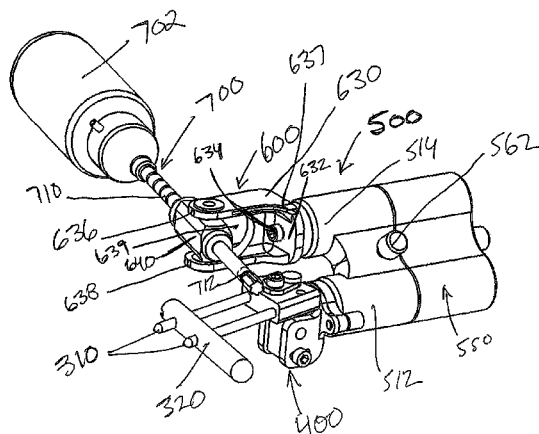
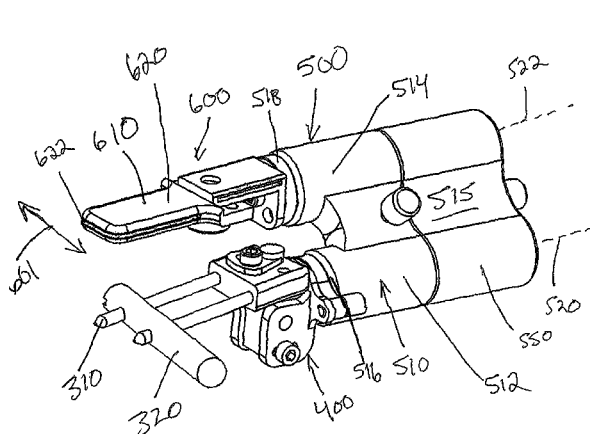
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(57) **ABSTRACT**

A system for guiding resurfacing operations on at least a
portion of a joint of at least one bone is provided and uses a
guide with actuators (motors) controlled by a computer to
position a cutting tool relative to a bone so that the bone
surface can be cut in a flexible and accurate manner.

31 Claims, 21 Drawing Sheets



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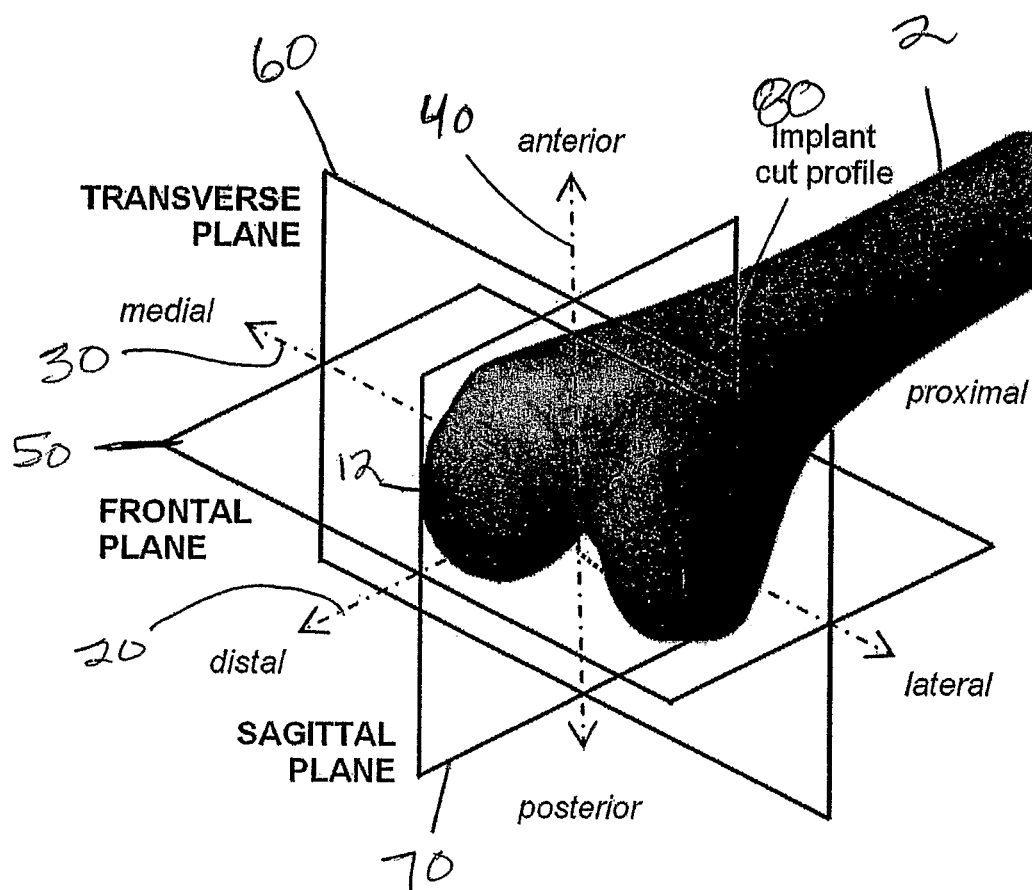
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FIG. 1



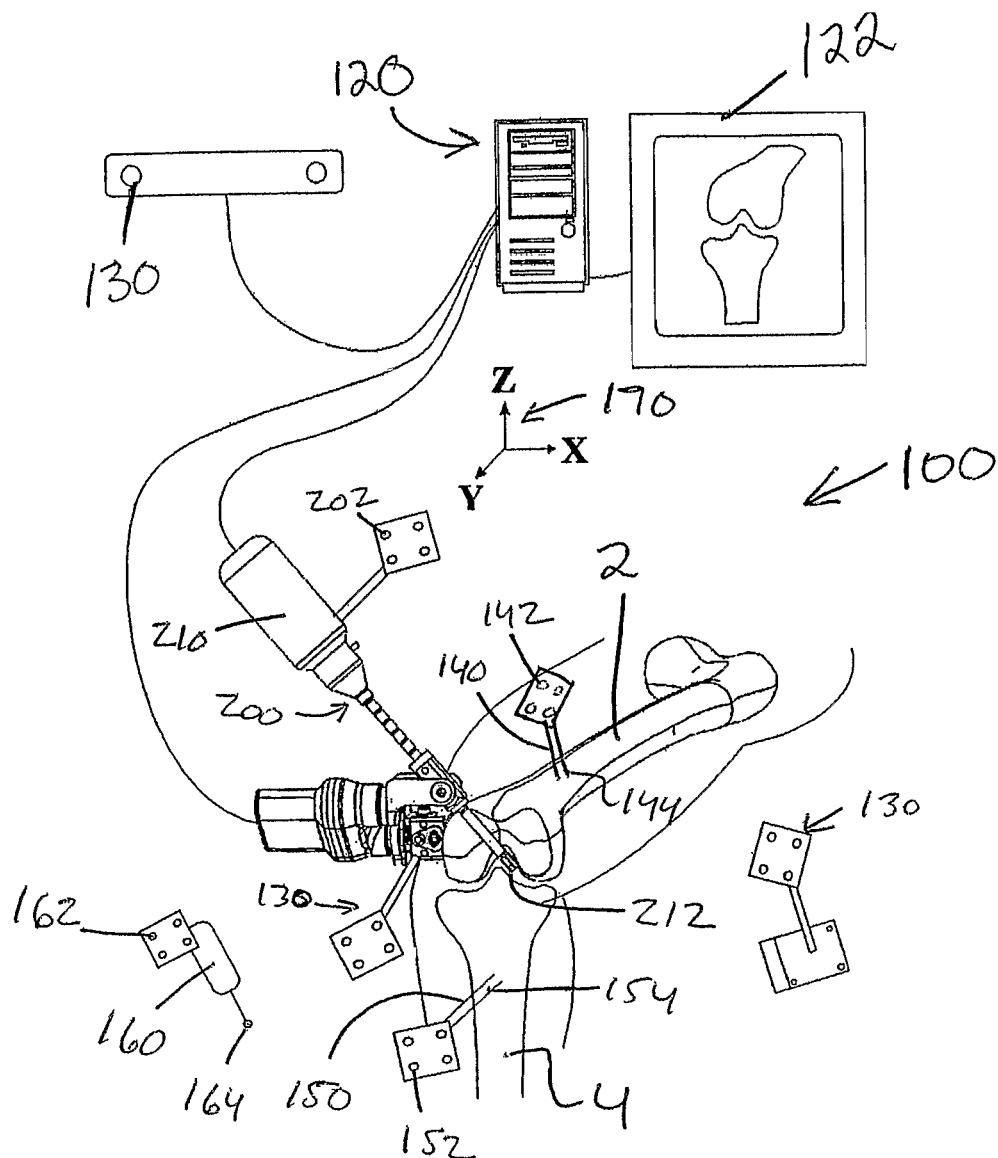
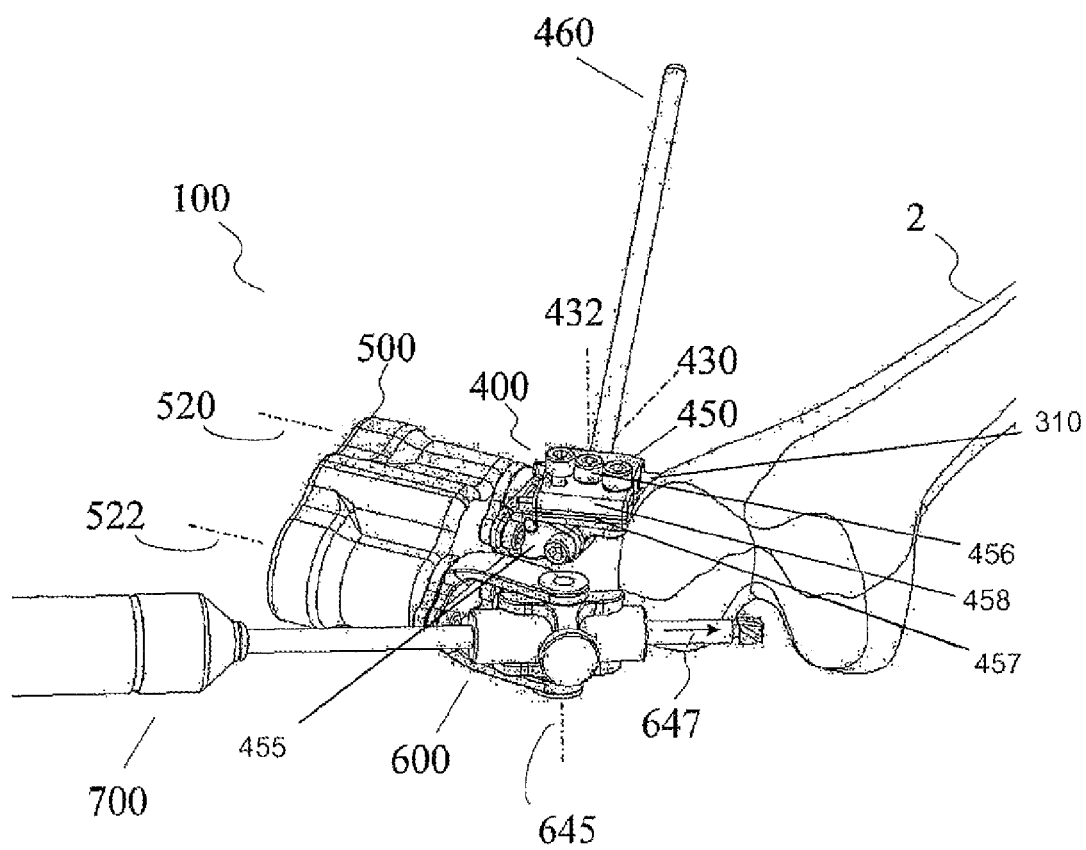


FIG. 2

FIG. 3



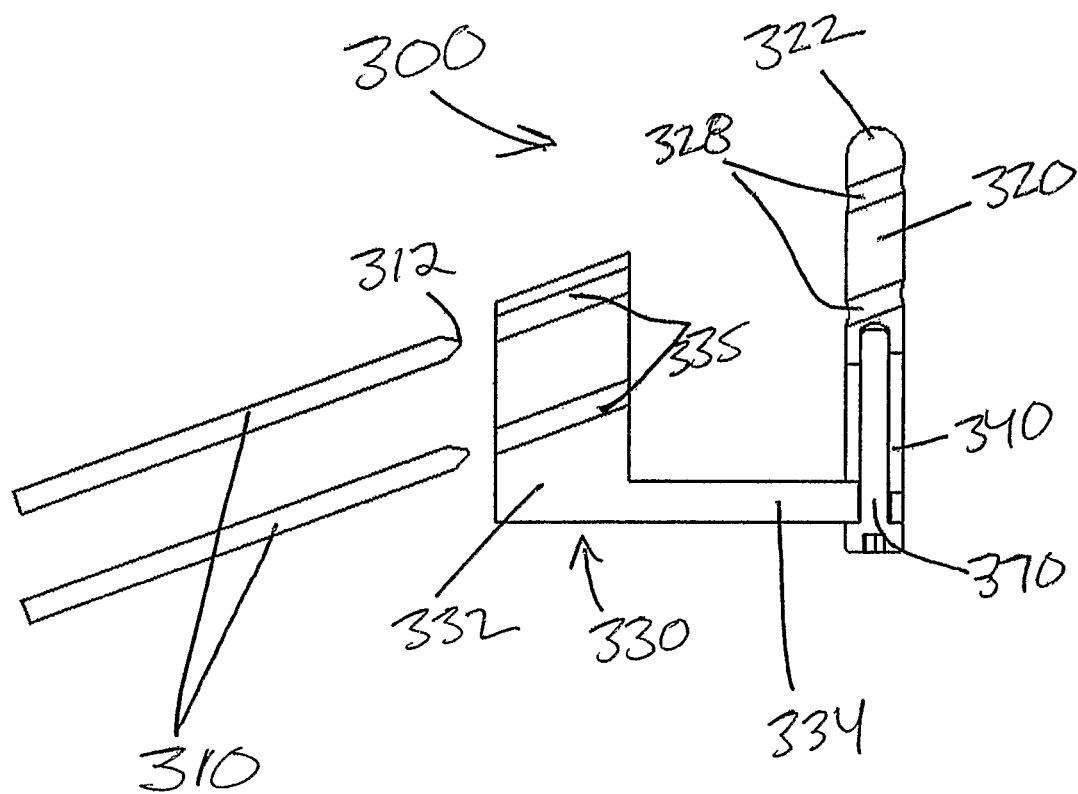
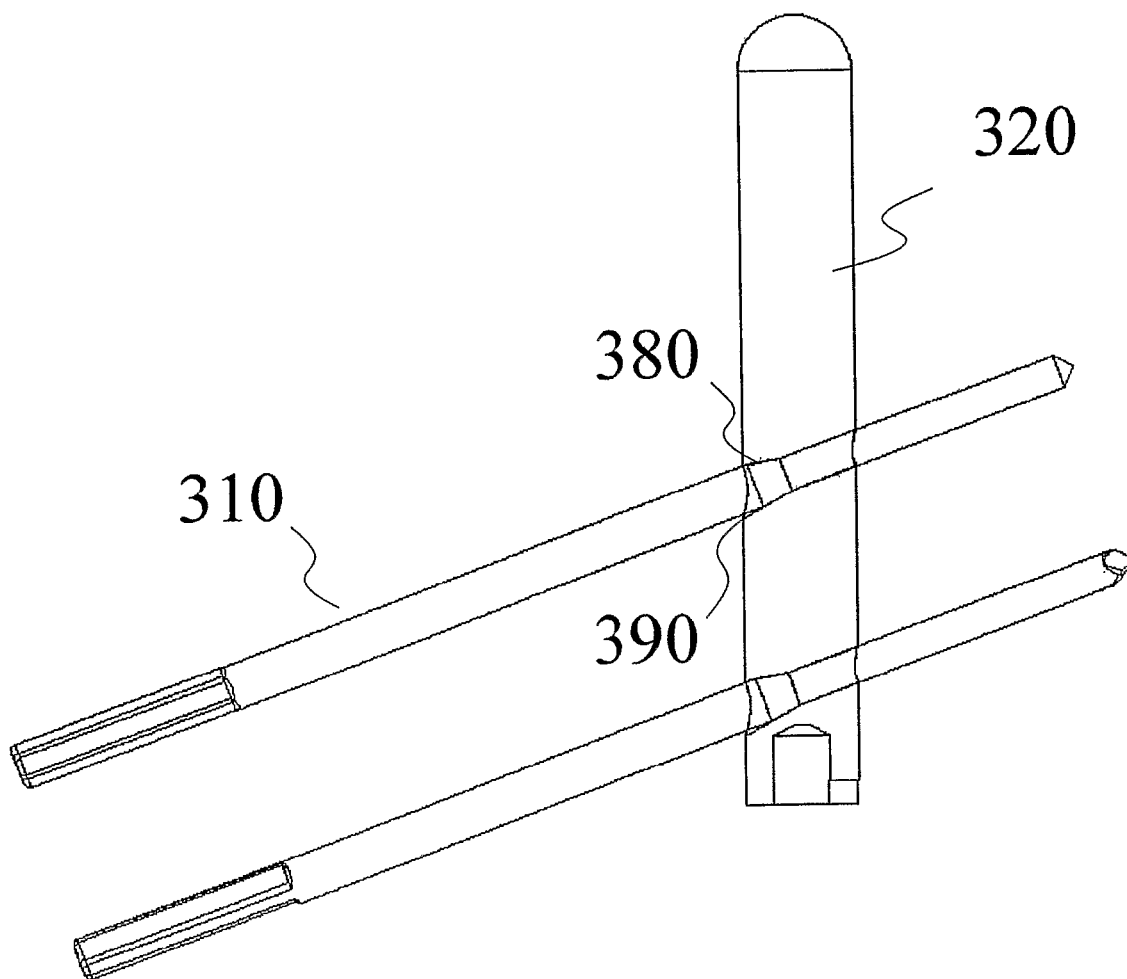


FIG. 4A

FIG. 4B

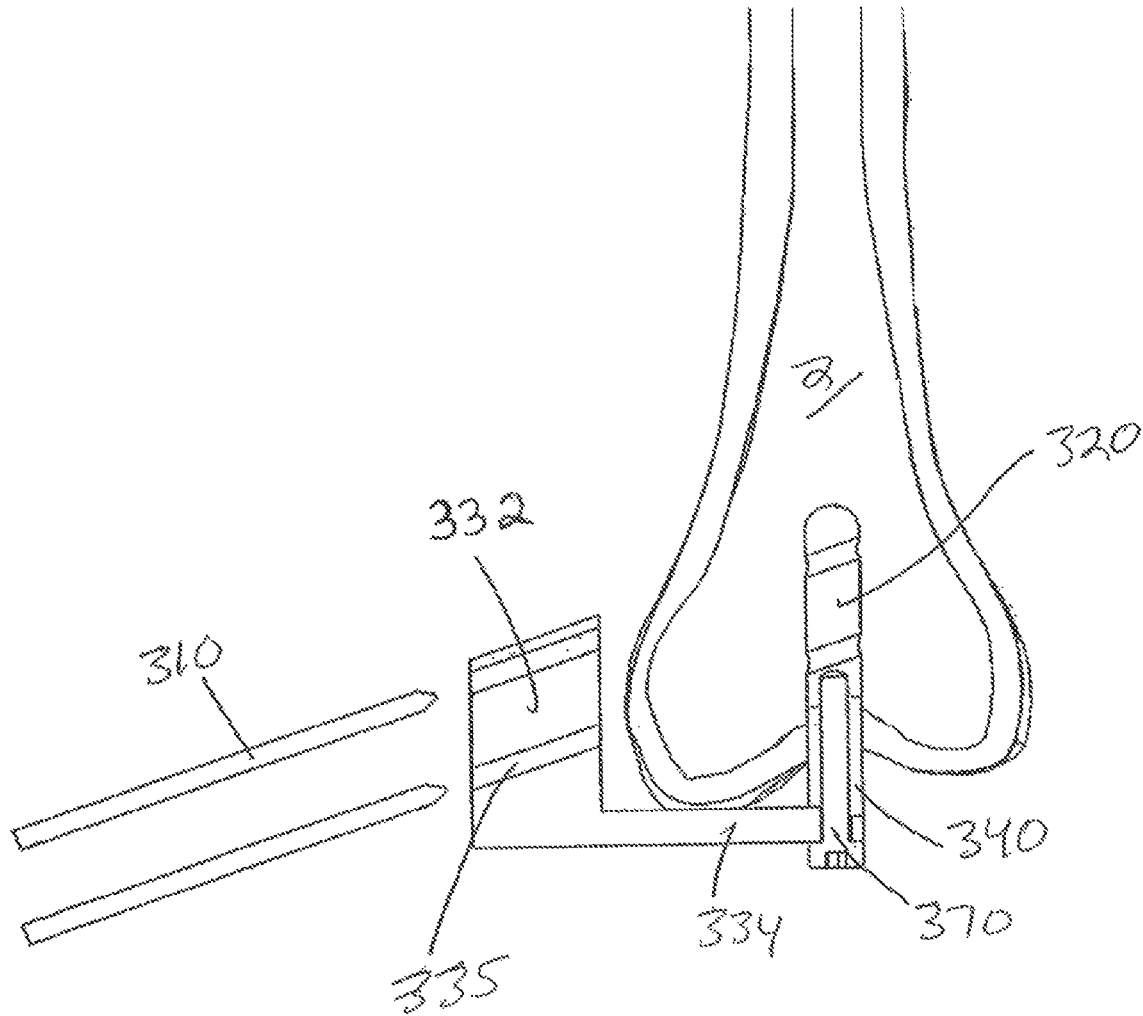


FIG. 5

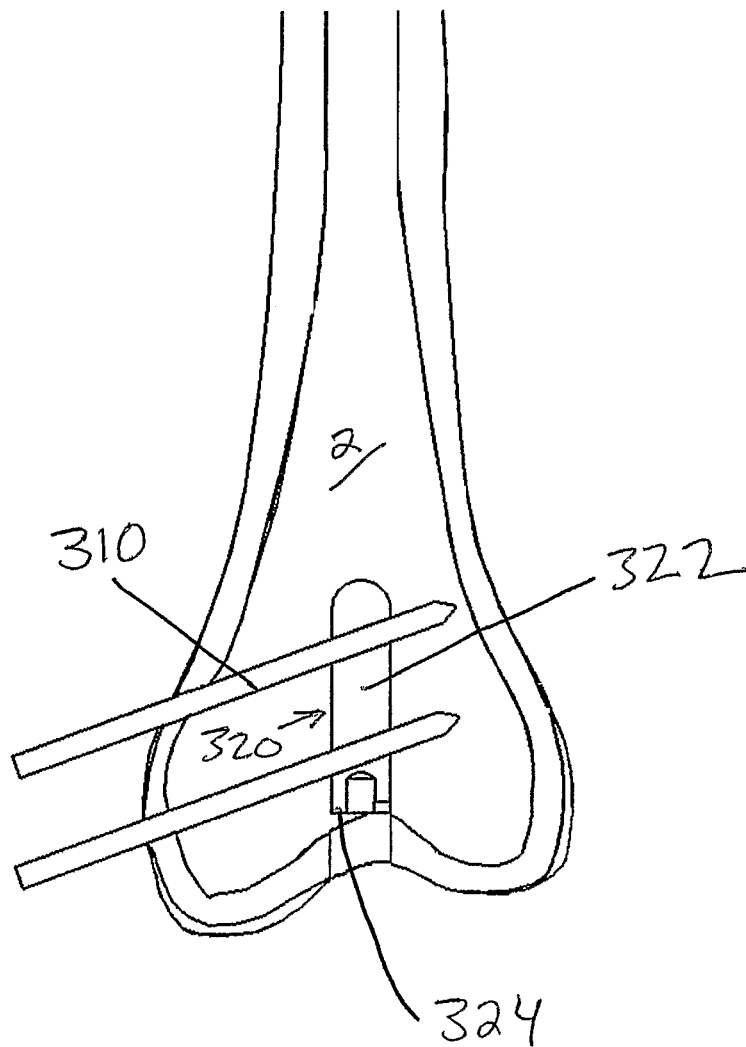


FIG. 6

FIG. 7

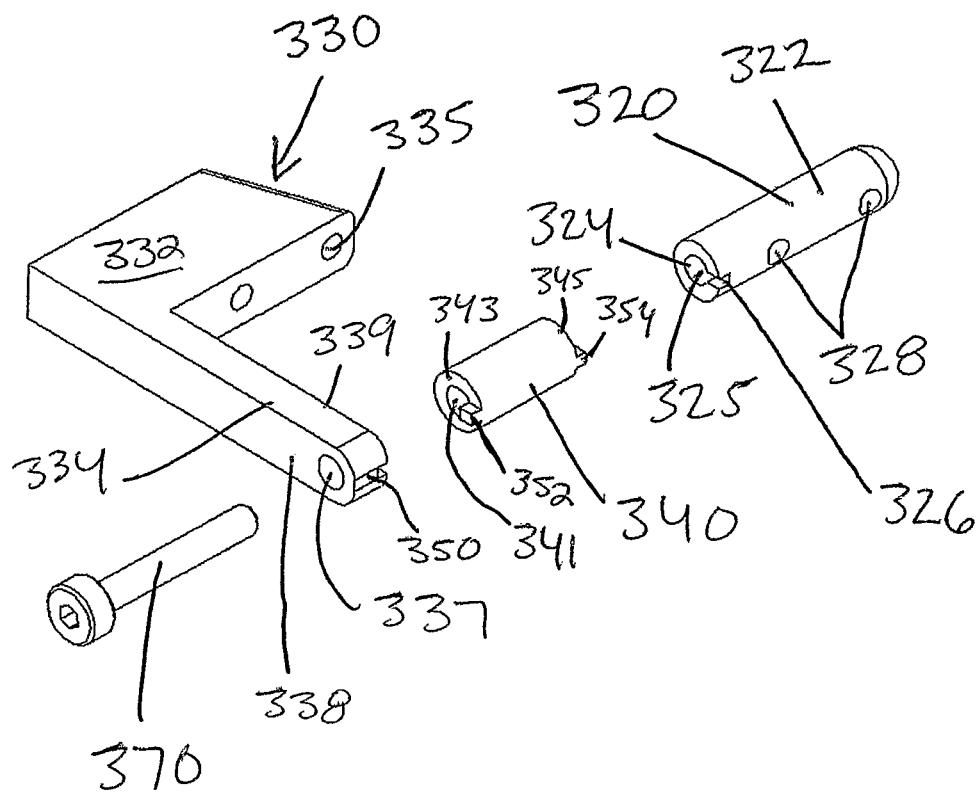


FIG. 8

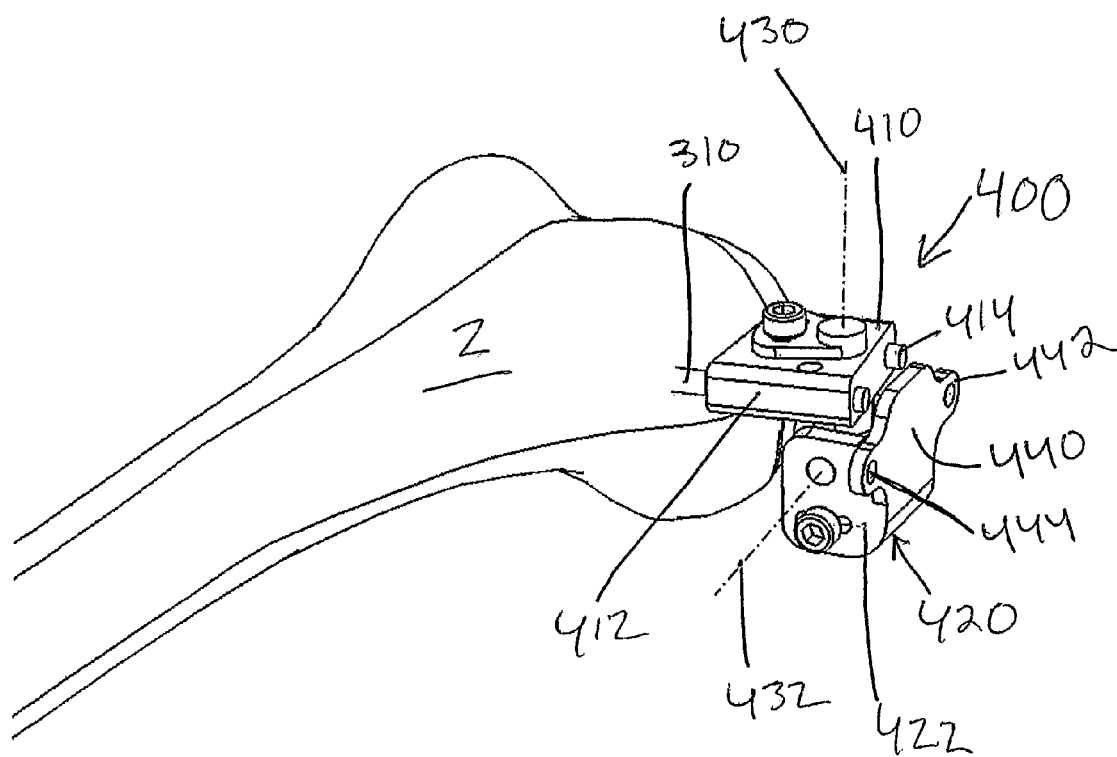


FIG. 9

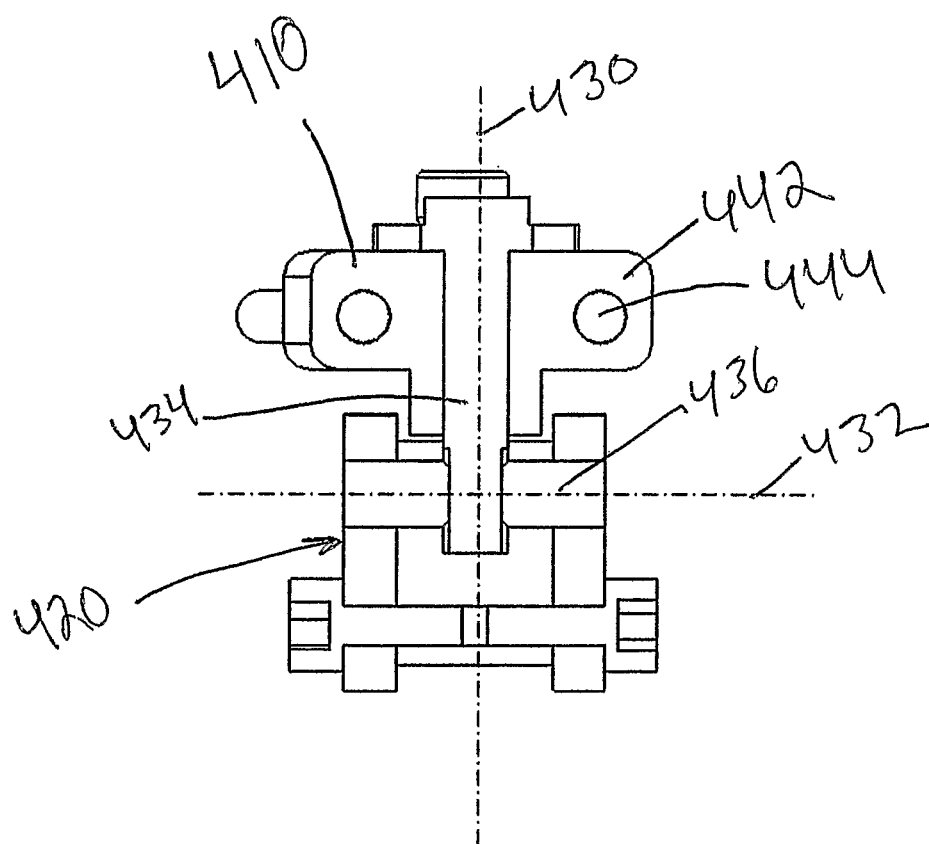
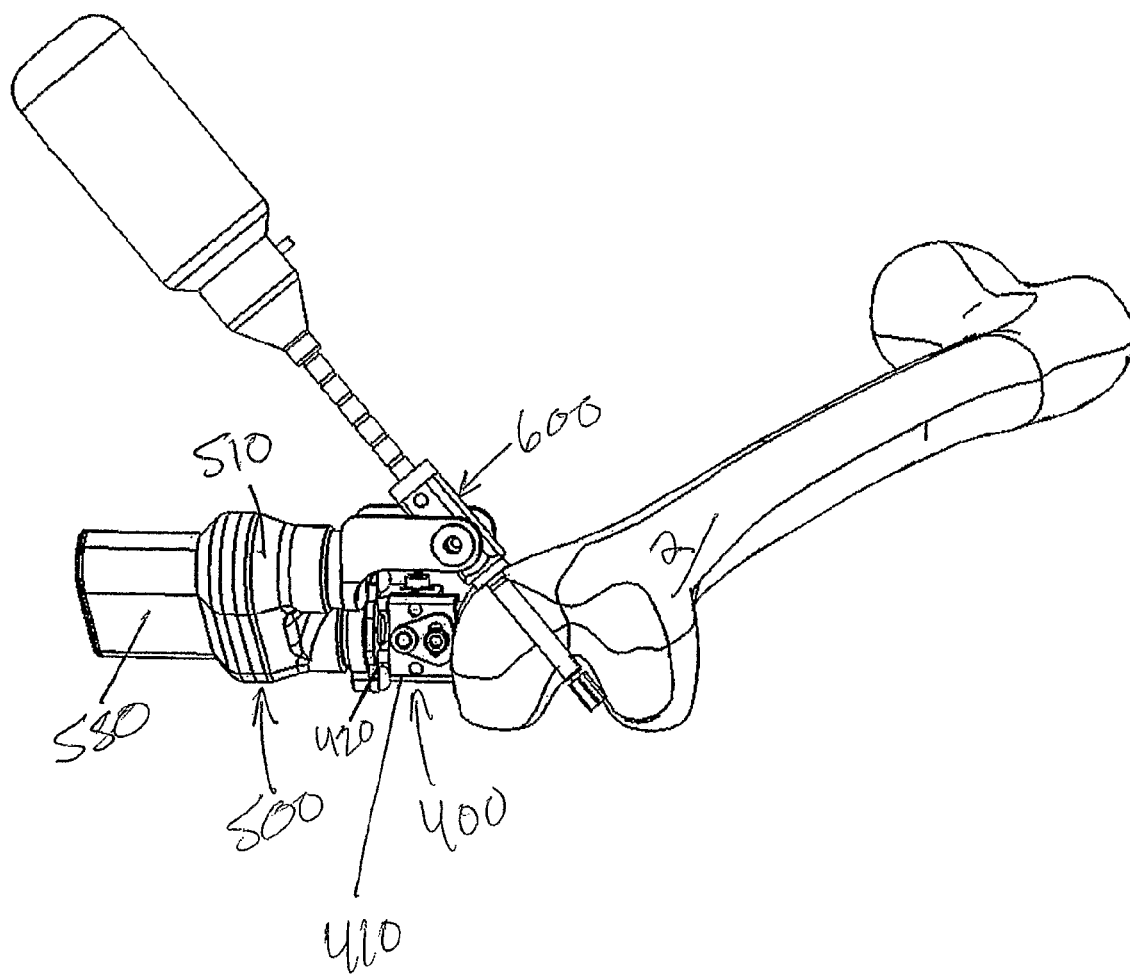


FIG. 10



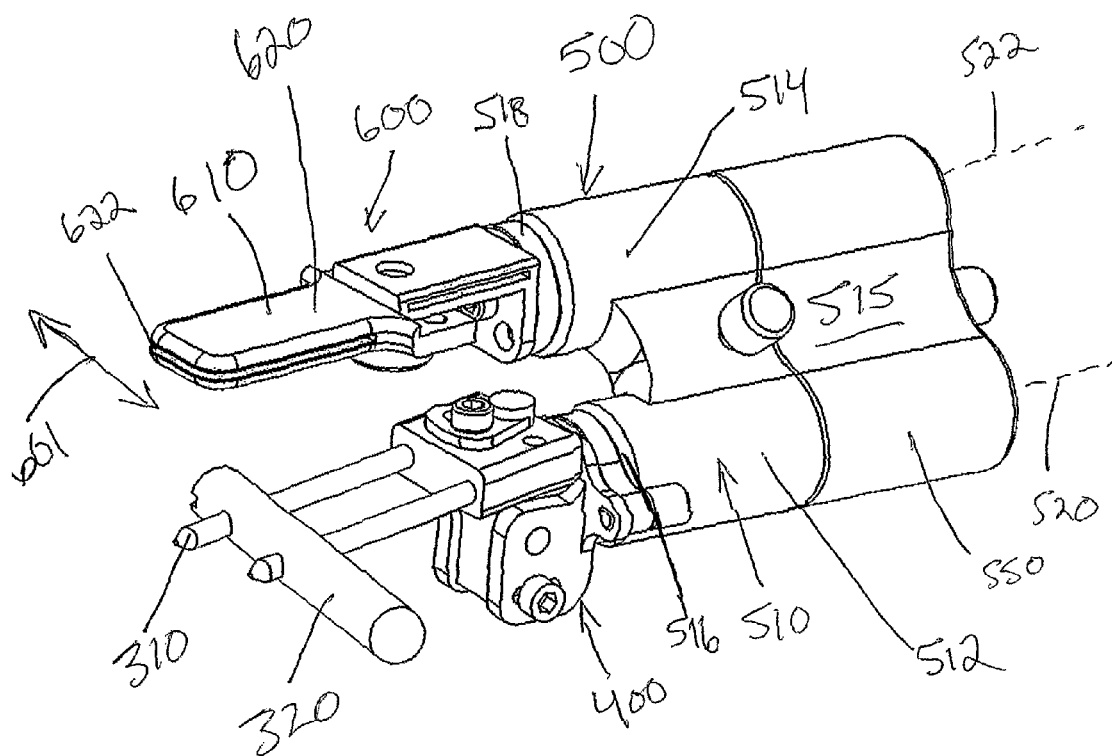


FIG. 11

FIG. 12

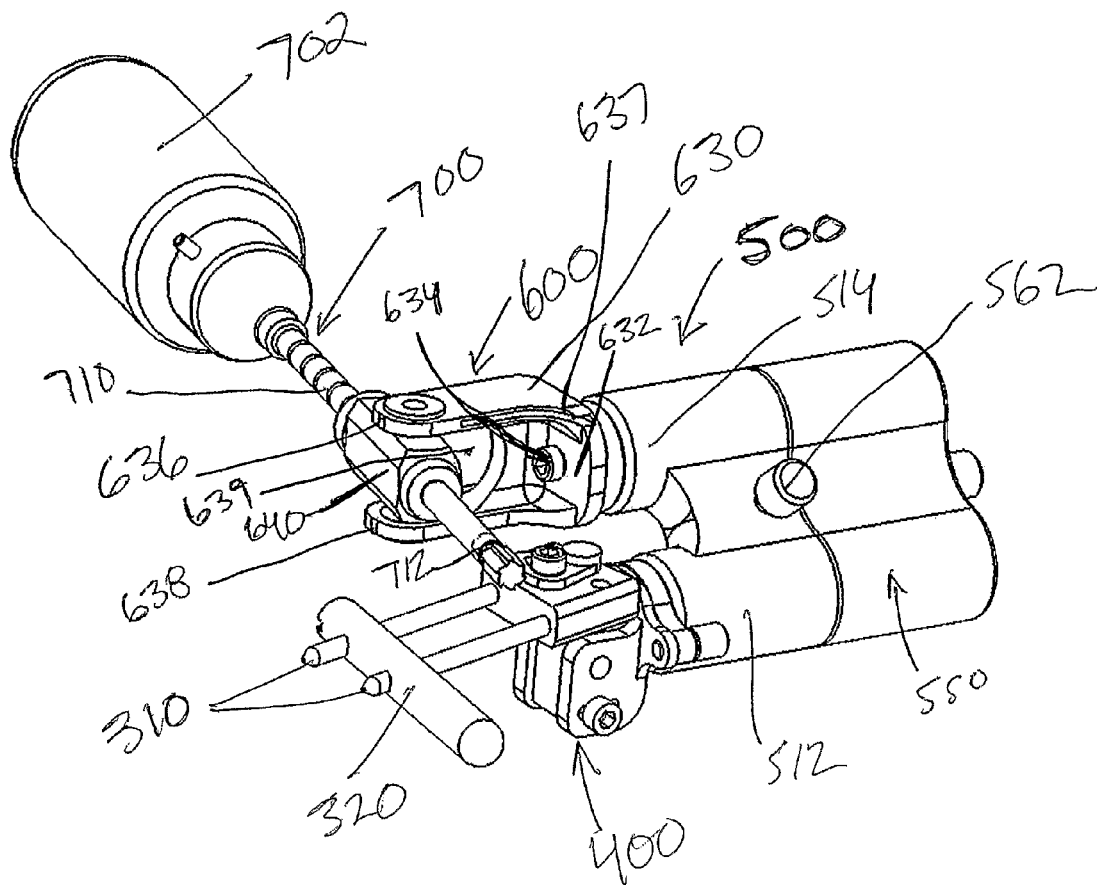


FIG. 13

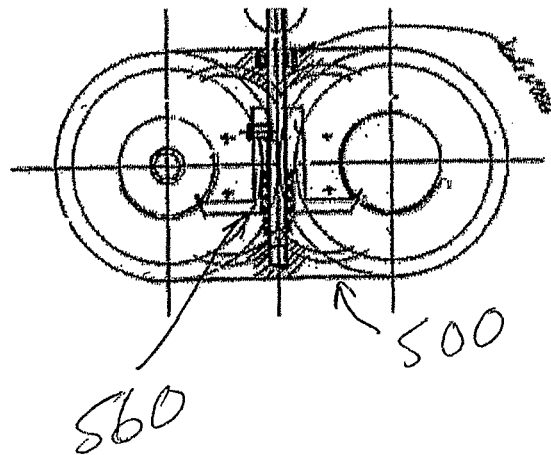


FIG. 14

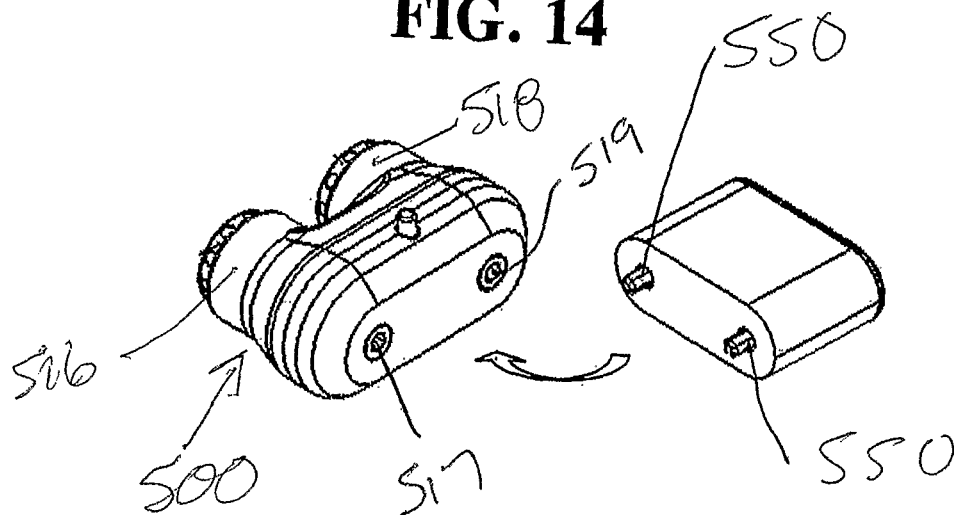


FIG. 15

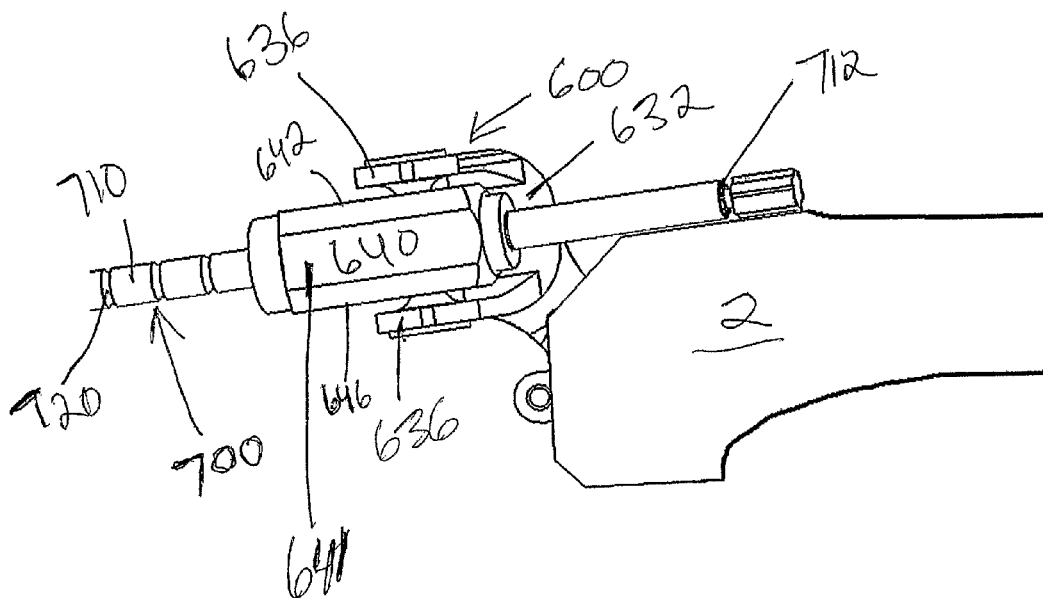
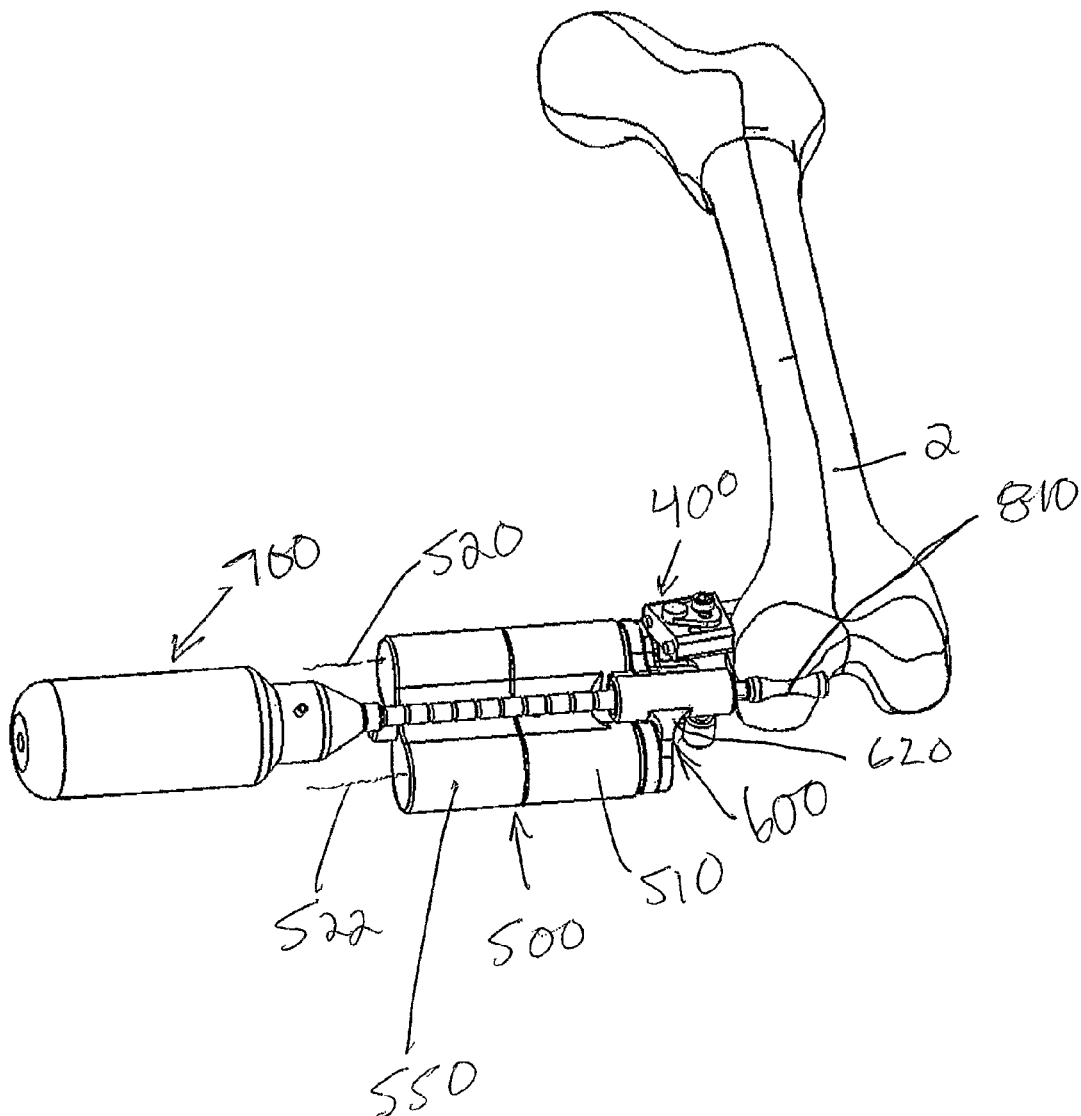


FIG. 16



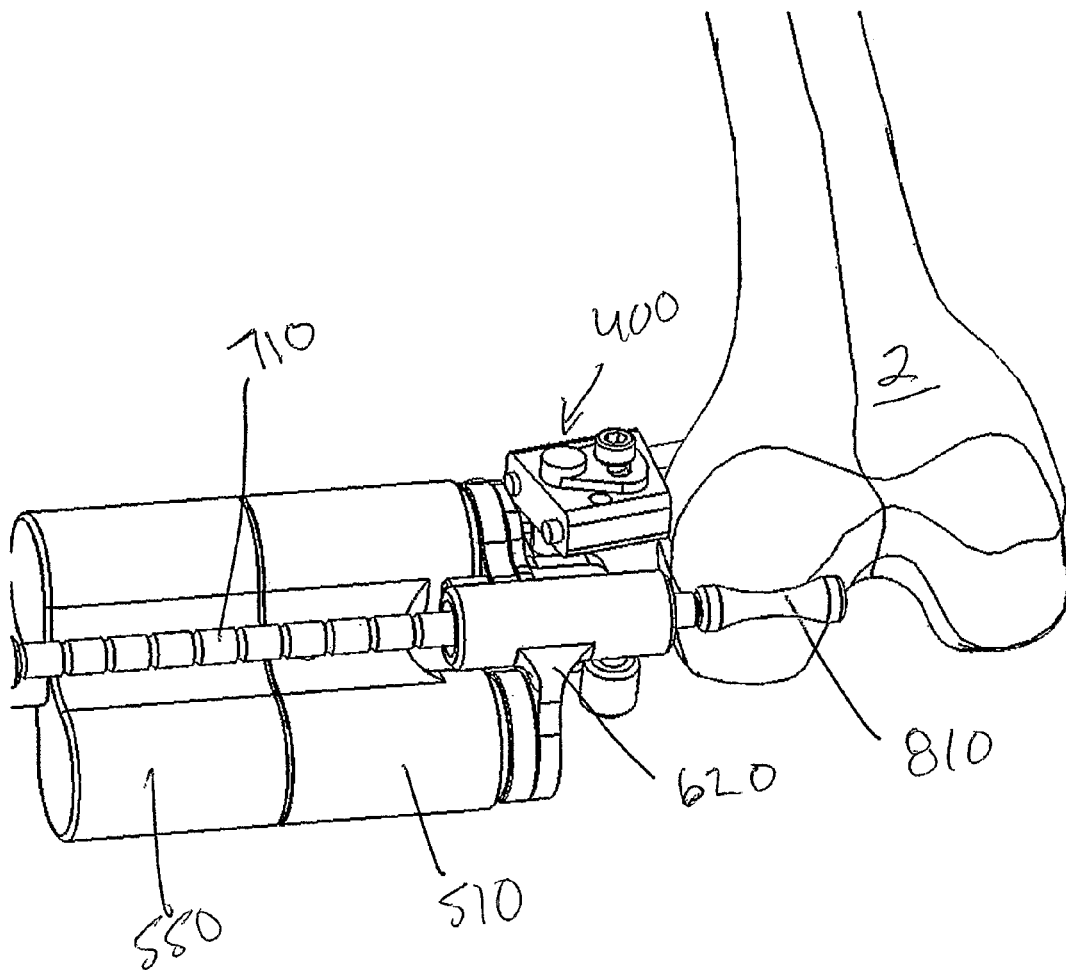
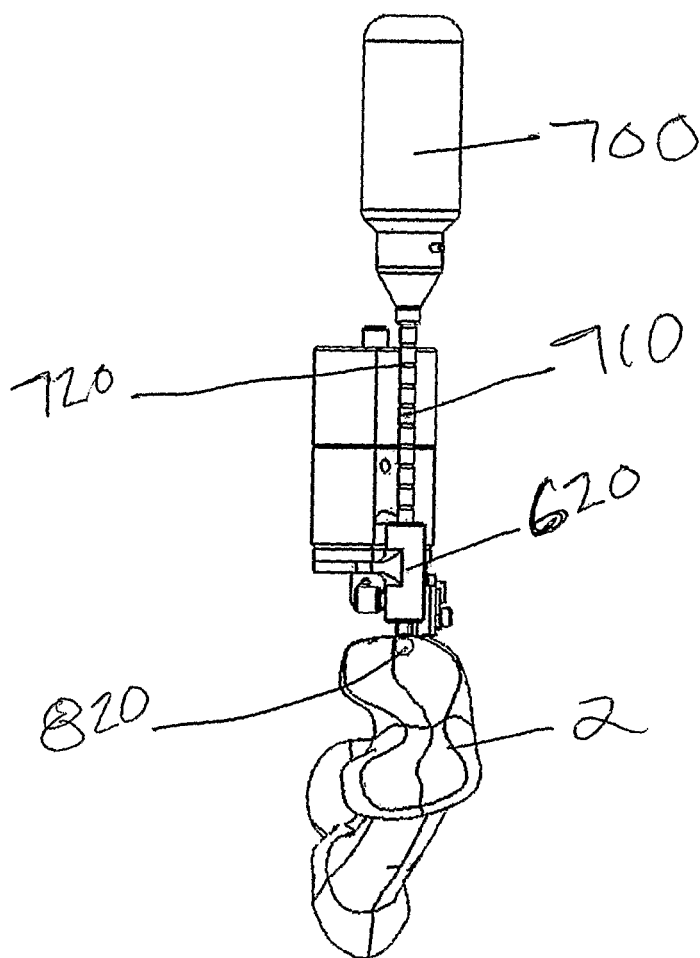


FIG. 17

FIG. 18



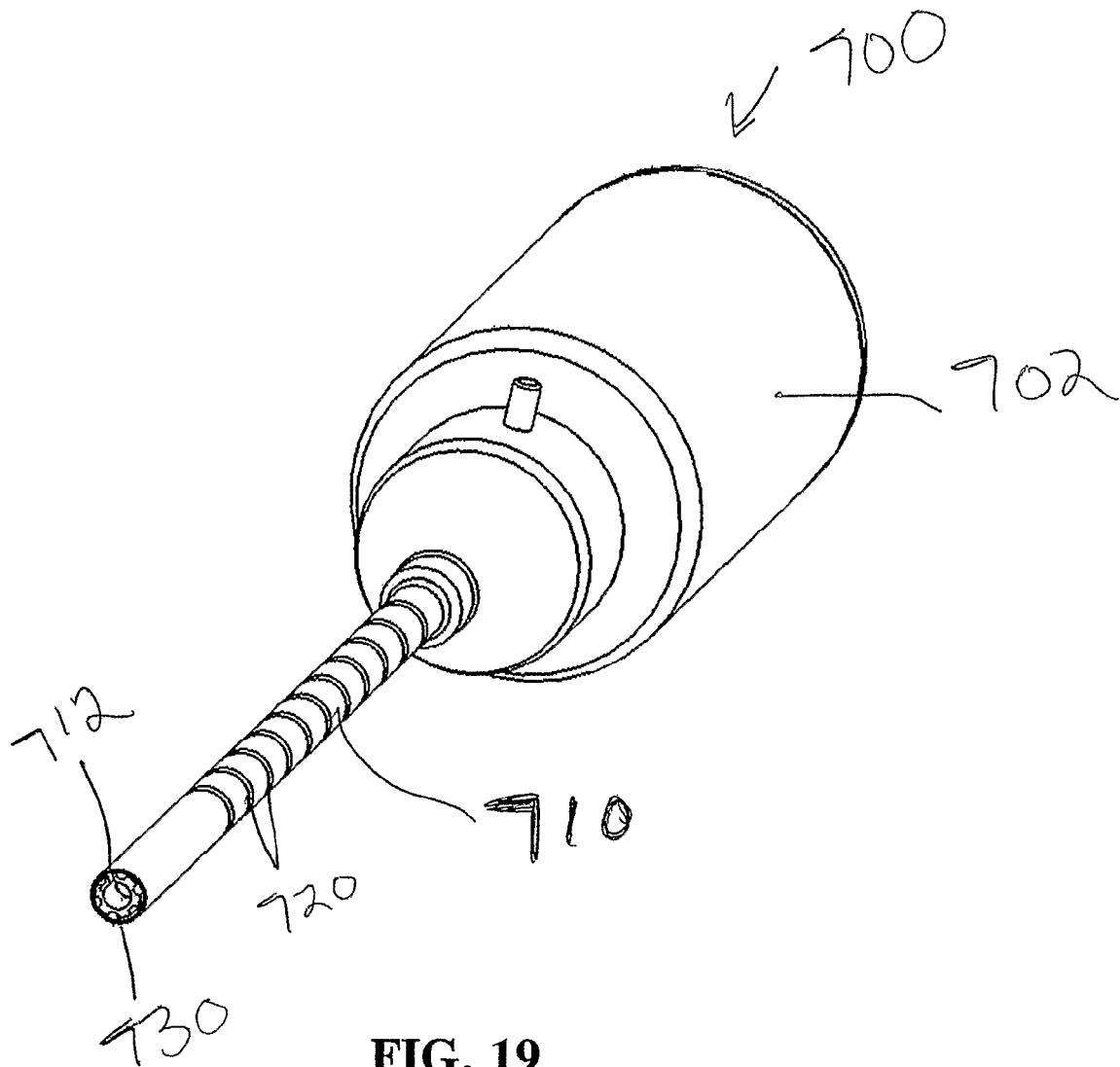


FIG. 19

FIG. 20

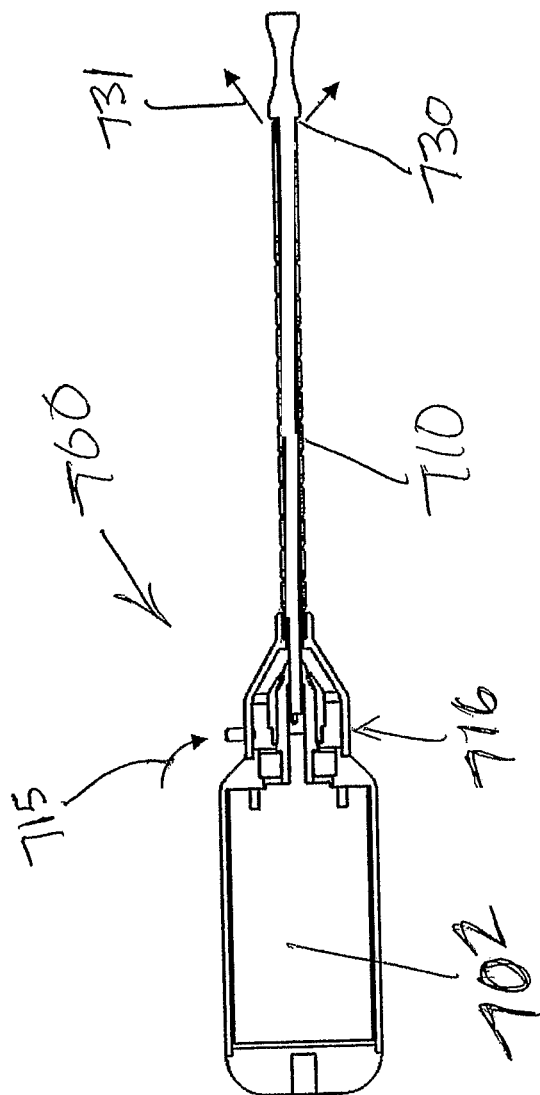
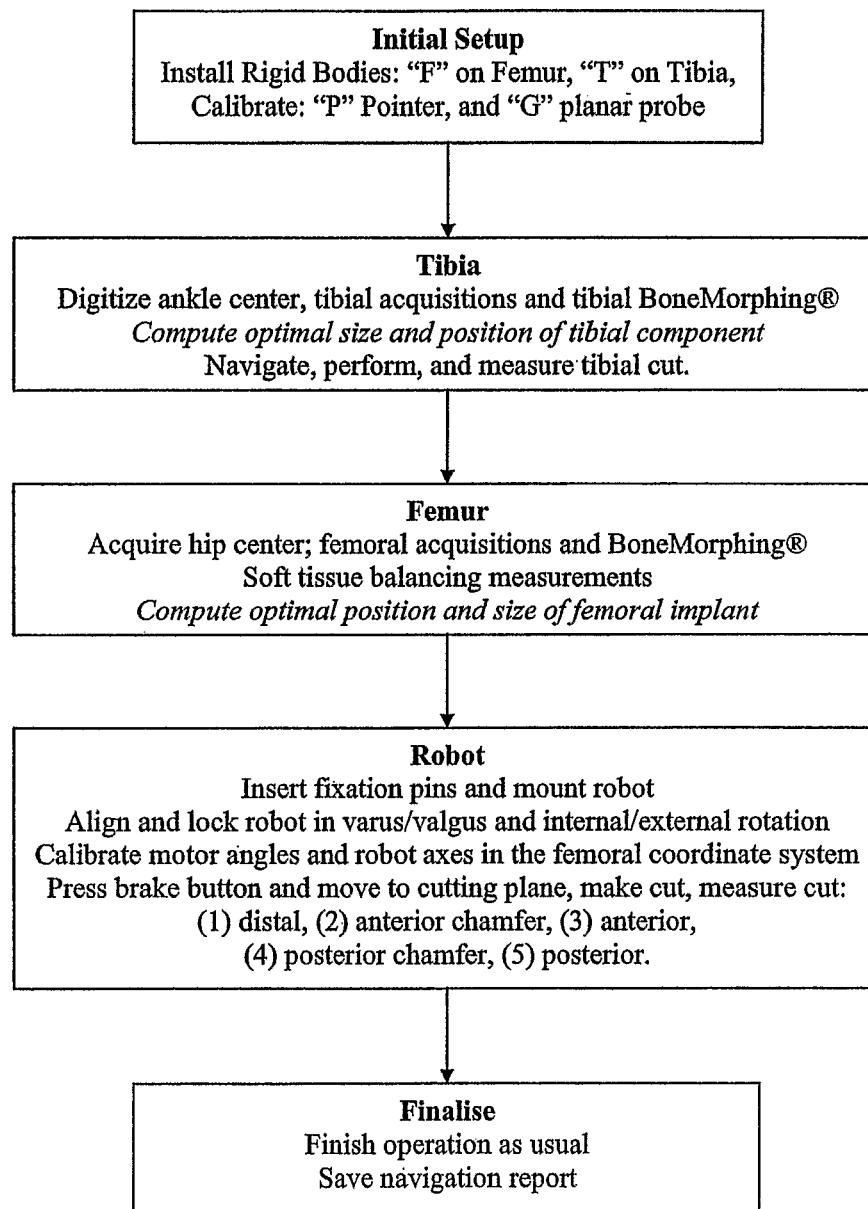


FIG. 21

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ROBOTIC GUIDE ASSEMBLY FOR USE IN COMPUTER-AIDED SURGERY

CROSS REFERENCE TO RELATED APPLICATION

This is a U.S. National Phase application under 35 U.S.C. §371 of International Application No. PCT/IB2006/000806, filed on Apr. 7, 2006, and claims the benefit of U.S. patent application Ser. No. 60/669,177, filed Apr. 7, 2006, both of which are hereby incorporated by reference in their entirety.

TECHNICAL FIELD

The present invention relates to a method and system for computer and robot aided surgery and more particularly, relates to a robot-aided guide assembly that has a guide mechanism and cutting tool for making precise bone cuts as part of a surgical procedure, such as joint replacement or resurfacing operations.

BACKGROUND

The World Health Organization estimates that there is currently several hundreds of millions of people suffering from bone and joint diseases, and this figure is projected to increase sharply due to the predicted doubling of the number of people over 50 by the year 2020.

Partial or total joint replacement or resurfacing is currently one of the most popular methods of treating for patients who suffer from bone and joint diseases, such as severe degenerative joint osteoarthritis or arthrosis. For instance, approximately 600,000 osteoarthritis patients worldwide undergo total knee arthroplasty (TKA) every year to relieve their joint pain and to restore their proper knee function with respect to joint loading and kinematics. Uni-compartmental knee arthroplasty (UKA), where only the medial or lateral condyles of the femur and tibia are replaced is also a popular and is a less invasive treatment for certain patients with knee osteoarthritis.

There are several different surgical techniques and forms of implants used for both TKA and UKA. In conventional TKA, for example, the surgeon strives to achieve accurate alignment by adequately exposing the knee joint, properly orientating cutting guide blocks across the exposed aspect of the bones from the anterior side of the knee, and sawing off the worn joint surface by using the block surface or slot to guide the oscillating saw-blade.

To adequately expose the knee joint, the standard approach used is a 25-30 cm skin incision extending proximally from just distal to the level of the tibia tubercle (known as the anterior or midline approach), followed by a medial 20-30 cm parapatellar arthrotomy, which extends superiorly through the quadriceps tendon. Although the extent of the incision allows for lateral eversion and dislocation of the patella, thus exposing most of the structures of the knee joint, dividing the distal third of the quadriceps muscle in this manner can have several potential repercussions for the patient. These include increased pain, blood loss, and time to ambulation (both with and without walking aids), prolonged post-operative hospital stay and rehabilitation, and decreased range of motion and knee strength in daily tasks, such as stair climbing and descending stairs, etc.

Minimally invasive surgical (MIS) techniques have been used only for uni-condylar knee arthroplasty for over a decade, though surgeons have only relatively recently begun to apply the principles of MIS to TKA. In this technique, the

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knee joint is accessed mainly from the side through a 6-9 cm incision instead of a 20-30 cm incision. Approaching bone cuts medially or obliquely instead of anteriorly circumvents the need to evert the patella and violate the quadriceps. This, in turn, reduces morbidity by reducing the trauma to the extensor mechanism, and improves post-operative knee function, recovery rate and pain.

In TKA, implant alignment and positioning is regarded to be one of the most important surgical variables for the long term success of the operation. Implant alignment and positioning can be described by the degrees of freedom associated with each implant. For the femoral component these include three rotations, namely, varus/valgus alignment, flexion/extension alignment, and internal/external or transverse alignment; as well as three positions, namely, anterior-posterior (AP) positioning, proximal-distal (PD) positioning and medial-lateral (ML) positioning. Most TKA femoral implants include an inner surface comprised of at least five planes. The five cutting planes that must be realized on the distal femur are the interior cut, anterior chamfer cut, distal cut, posterior chamfer cut and posterior cut. Other inner implant geometries consist of curved surfaces.

In order to accommodate these different surgical techniques and implants, there exists several different types of bone-cutting or resurfacing guides. These can range from rigid mechanical jigs, to mechanized systems, to robotic cutting guides. Some of these conventional guides are disclosed in U.S. Pat. Nos. 6,858,032 and 5,228,459; U.S. application publication No. 2005/0055028 and German patent No. DE 203036643, all of which are hereby incorporated by reference in their entireties.

Most of the above conventional systems use some type of template to guide a cutting tool. However, all of these conventional systems suffer from a number of deficiencies and in particular, these systems do not provide all of the following desired features: accuracy with respect to global implant positioning; accuracy with respect to bone cut surface reproducibility; flexibility in terms of implant type; flexibility in terms of inner implant surface complexity, geometry and size; compatibility with minimal access approaches; compactness; simplicity and ease-of use.

SUMMARY

The present invention relates to a system for guiding resurfacing operations on at least a portion of a joint of at least one bone. The system uses a guide with actuators (motors) controlled by a computer to position a cutting tool relative to a bone so that the bone surface can be cut in a flexible and accurate manner.

The system of the present invention includes a number of components that cooperate with one another to perform the intended guide and cutting operations. In particular, the system can include fixation instrumentation, an orienting apparatus, a positioning mechanism, and a guide assembly for guiding a cutting or milling tool.

According to one embodiment, a system for guiding a cutting tool capable of cutting bone portions at a level of a head of a bone is provided and includes (a) means for attaching the system to only one side of the bone through an incision in the bone; (b) an adjustment mechanism rotatably coupled to the attachment means for adjusting the position of the cutting tool; (c) a positioning mechanism coupled to the adjustment mechanism and having at least two degrees of rotational freedom for further adjusting the position of the cutting tool; and (d) a guide intended to support the cutting

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tool and pivotally coupled to the positioning mechanism along one axis of rotation of the positioning mechanism.

These and other features and aspects of the invention can be appreciated from the accompanying figures and the following description.

BRIEF DESCRIPTION OF THE DRAWING FIGURES

The foregoing and other features of the present invention will be more readily apparent from the following detailed description and drawings of the illustrative embodiments of the invention wherein like reference numbers refer to similar elements and in which:

FIG. 1 is a perspective view of an anatomical coordinate system of a knee;

FIG. 2 is a perspective view of a computer and robot assisted surgery system;

FIG. 3 is a robotic system for guiding joint replacement and resurfacing operations on at least a portion of a point of at least one bone;

FIG. 4a is a side elevation view, in cross-section, of a fixation instrument for use with a guide system of the robotic surgery system of FIG. 3;

FIG. 4b is a side elevation view, in cross-section, of a variation of the fixation instrument of FIG. 4a.

FIG. 5 is a side elevation view, in cross-section, of the fixation instrument of FIG. 4a inserted in a distal femur;

FIG. 6 is a side elevation view, in cross-section, of the fixation instrument inserted in the distal femur with a pin guide removed;

FIG. 7 is an exploded perspective view of a pin guide and anchor of the fixation instrument of FIG. 4a;

FIG. 8 is a perspective view of an orienting apparatus of the guide system of the computer assisted surgery system of FIG. 3 fixed to a side of the distal femur;

FIG. 9 is a cross-sectional view of the orienting apparatus of FIG. 8;

FIG. 10 is a perspective view of a positioning mechanism attached to the orienting apparatus with a milling system attached thereto for performing resurfacing operations on the bone;

FIG. 11 is a perspective view of the positioning mechanism of FIG. 10 attached to the orienting apparatus with a sawing guide attached thereto;

FIG. 12 is a perspective view of the positioning mechanism of FIG. 10 with the orienting apparatus and a milling system attached thereto, as well as the fixation instrument;

FIG. 13 is a cross-sectional view of one exemplary brake mechanism for the positioning mechanism;

FIG. 14 is a perspective view showing the modular nature of the positioning mechanism;

FIG. 15 is a side perspective view of the milling system milling the anterior cut plane with a straight side cutter;

FIG. 16 is a perspective view of the milling system and guide system, with the milling system milling with a curved side cutter that conforms to the curved inner shape of the implant;

FIG. 17 is a close-up perspective of the system of FIG. 16;

FIG. 18 is a perspective view of the milling system milling with a ball end cutter;

FIG. 19 is a perspective view of a milling tool of the milling system;

FIG. 20 is a cross-sectional view of the milling tool of FIG. 19 illustrating a milling irrigation system; and

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FIG. 21 is a flow chart of an exemplary surgical procedure using the guide system of the present invention in a joint replacement (TKA) operation.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

Referring now to FIG. 1, a perspective anatomical coordinate system of the knee is illustrated. More specifically, a bone 2 (e.g., femur) is shown and includes a distal end 12. A proximal/distal axis 20 is provided to show proximal and distal directions relative to the femur 2. In addition, a medial/lateral axis 30 is provided to show the medial and lateral portions of the femur 2 and an anterior/posterior axis 40 is provided to show the anterior and posterior portions of the femur 2. To assist in performing resurfacing and cutting operations on the femur 2, several reference planes are provided. In particular, a frontal plane 50 is provided, a transverse plane 60 is provided, and a sagittal plane 70 is provided. For purpose of illustration only, an implant cut profile 80 is illustrated and projected onto the sagittal plane 70 to illustrate the five planar cuts of a typical total knee arthroplasty (TKA) femoral implant.

Referring now to FIG. 2, a computer-assisted orthopedic surgery (CAOS) system 100 is schematically shown. The system 100 is configured for performing joint replacement or resurfacing operations, such as TKA. The system 100 can be used to plan the optimal position of an implant, such as a knee implant, relative to the bone 2, 3, and to position a guiding system such that the final cut surface corresponds to the planned implant position cut surface.

The system 100 includes a suitable position measuring device 110 that can accurately measure the position of marking elements in three dimensional space and in the case of a knee implant, the device 110 includes at least one bone, such as the patient's femur 2 or tibia 4. The position measuring device 110 can employ any type of position measuring method as may be known in the art, for example, emitter/detector or reflector systems including optic, acoustic or other wave forms, shape based recognition tracking algorithms, or video-based, mechanical, electromagnetic and radio frequency systems. In a preferred embodiment, schematically shown in FIG. 2, the position measuring system 110 is an optical tracking system that includes at least one camera that is in communication with a computer system 120 and positioned to detect light reflected from a number of special light reflecting markers, such as spheres or discs 130. The computer system 120 includes a display 122 to permit visual display of the images.

Detecting and determining the position and orientation of an object is referred to herein as "tracking" the object. To provide precision tracking of objects, markers 130 can be rigidly connected together to form reference bodies, (e.g., 140, 150), and these reference bodies can be attached to bones, tools and other objects to be tracked. One such device that has been found to be suitable for performing the tracking function is the Polaris™ system from Northern Digital Inc., Ontario, Canada. Objects to be tracked thus typically include at least three markers (or triplets), which can be configured to emit, receive, or reflect energy, such as light or acoustic energy.

The position measurement device 110 is described in greater detail in a number of publication, including U.S. patent application Nos. 20050101966 and 11/299,287, both of which were previously incorporated by reference.

To sense the position of light reflecting markers, the system 100 includes at least two detecting elements, such as two

cameras. The two cameras detect the light reflected from the light reflecting markers to determine the position of each marker associated with the tracked object, the position and orientation of the tracked object are also determined.

The position of the patient's bones, such as the patient's femur **2** and the patient's tibia **4**, can be determined and tracked by attaching reference bodies **140**, **150**, which include respective markers **142**, **152**. Reference bodies can be attached to bones or tools using pins or screws (**144**, **154**), or various quick release mechanisms. The reference bodies can also be shaped in the form numbers (e.g., "1", "2", "3"...) or alphabetical letters, such as "F" for Femur, "T" for Tibia, "P" for pointer, and so on, so as to avoid confusion as to which reference body should be attached to which bone or tool.

The tracked objects and their relative positions can be displayed on a screen that is connected to the computer system **120**. In a preferred embodiment, the display is a touch screen which can also be used for data entry.

The position measurement device **110** includes a number of different tools that are used at different locations and perform different functions as the system **100** is operated to yield optimal joint reconstruction data and information. These tools include the above described markers, which act as landmark markers, as well as other tools as will be described in greater detail below, such as a milling or cutting system **200** having at least three markers **202** is an example of an object trackable by position measuring device **110**. The system also includes a pointer **160**, with markers **162**, which can be used to digitize points on the surfaces of the femur **2** and tibia **4**. The system **100** can further include a calibration device that can be used to measure the relationship between a pointer tip **164** and the markers **162**. Accordingly, the markers **162** permit the position or the pointer tip **164** to be determined from the positions of the markers **162** relative to the three-dimensional coordinate system **170**.

For sake of simplicity and with respect to the discussion of FIG. **2**, the system **200** is described as including a milling or drilling device or any other type of cutting device **210** also has a tip **212** having a known spatial relationship relative to markers **202**. Position measuring device **110** determines the position and orientation of markers **202** in the three dimensional coordinate system **170**. Based upon the known spatial relationship between the tip **212** and markers **202**, the position of the tip **212** is determined.

Computer **120** is optionally configured to allow at least one of medical image data and ultrasound data to be used in planning the position and orientation of an implant in a bone. The trajectory or path of a cutting surface being milled by the device **210** can be monitored and displayed by the computer **120**. Thus, the actual path can be compared to the previously planned cut path to allow the practitioner to verify that there is no deviation between the actual procedure and the preoperative plan. In one embodiment, the device **210** is guided to allow the computer **120** to control the milling or drilling path.

The system **100** also includes a plurality of reference bodies **140**, **150**, for determining the position and orientation of an individual's bone in the three dimensional coordinate system **170**. The reference bodies **140**, **150** are preferably rigid and include respective markers **142**, **152**, which are preferably configured to emit or reflect energy. Each reference body **140**, **150** preferably includes a respective attachment element, such as pins or screws **144**, **154**, with which the reference bodies can be releasably attached to a bone. For example, the reference body **140** can be attached to femur **2**. The position and orientation of femur **2** can be determined based upon the position and orientation of markers **142** attached thereto.

Markers **142**, **152** are sufficient to establish the position and orientation of the rigid bodies **140**, **150** within the coordinate system **170**.

The system **100** also includes the pointer **160** and can include an endoscope in some applications, which cooperate to allow a practitioner to digitize landmarks of the femur **2** and tibia **4**. Digitizing a landmark comprises determining the position of the landmark in the three dimensional coordinate system, as discussed below. The pointer **160** preferably includes a pointer tip **164** having a known spatial relationship to the markers **162**. Based upon the known spatial relationship, the position of the pointer tip **164** can be determined from the position and orientation of the markers **162**.

The system **100** can further include a planar probe that includes at least one planar surface for measuring the position and orientation of the planar probe to be determined. Moreover, a calibration system is preferably provided to measure the relationship between at least one of the planar surfaces on the probe and the markers. This relationship can also be determined by using the pointer **160** to point to and locate at least three points on the planar surface. Alternatively, the three points can have any known spatial relationship relative to the planar surface. Thus, the position of the planar surface can be determined from the positions of the markers relative to the three-dimensional coordinate system **170**. In addition, other planar surfaces can be in a known relative position with respect to the calibrated planar surface or the three or more located points.

In a preferred embodiment of the invention landmark points and or directions are digitized with respect to the femur **2** and tibia **4** with the pointer and are stored in the computer. Preferably an anatomical coordinate system for the femur and the tibia is defined based on at least a portion of the acquired data. The coordinate system could also be defined at least partially using kinematic methods, such as fitting a plane to a trajectory (e.g. fitting the sagittal plane **70** to the flexion/extension trajectory). Possible landmark points include but are not limited to the tibial plateau glenoids, spine, malleoli, the femoral notch, condyles, hip center, bone surface areas, etc.

Now referring to FIGS. **2-20**, the surgical system **100** is preferably an integrated system in which each of the tools is in communication with a master controller, such as the computer **120**, which serves to collect all of the data from the individual tools and then process the data to calculate various measurements that are displayable to the physician. The system **100** accordingly includes a user interface that is supported by software in the computer **120**. The user interface is configured to assist and walk the physician through the surgical procedure(s) to obtain optimal results and to assist the physician in determining what the best course of action is in terms of performing joint resurfacing and bone cutting operations.

To perform computer assisted orthopedic surgery, especially joint replacement or resurfacing, using the present system **10**, the reference body **140** is attached to the femur **2** at a selected point, as by screwing the reference body **140** into the bone with screws **144**. The reference body **140** includes the first set or triplet of markers **142** that are thus fixed to the femur **2** at the point. Similarly, the reference body **150** is attached to the tibia **4** at a selected point by screwing the body **150** into the bone with screw **154**. The reference body **150** includes the second set or triplet of markers **152** that are likewise fixed to the tibia **4**. Since the reference bodies **140**, **150** are fixed to the bones **2**, **4**, the pointer tip **164** can be used to point at any given point on bone **2**, **4**, the position of which is precisely taken by its tip **164**. Then, it is possible using a

conventional data processing system to determine the vector connecting the point where the respective body **140**, **150** attaches to the bone **2**, **4** to the point of the tip **164**, and therefore, locate any given point for any position of the femur **2** or tibia **4**.

According to one exemplary method, a number of different reference points are obtained. For example, the pointer tip **164** is used to digitize certain surfaces of the tibia **4**. Acquisition or data points are also taken for the femur bone **2** and more particularly, the pointer **160** is moved along the distal surfaces of the femur bone **2**. In all of these steps, the digitization occurs by locating and logging a selected bone surface point in the three dimensional coordinate system **170** and by using the data processing system. In other words, the pointer tip **164** is moved along the bone surface and coordinate data are gathered for use in generating a morphological model of that bone portion. The pointer **160** can be actuated to begin data acquisition by simply activating an actuator, such as a foot pedal in which case it is merely depressed by the physician. The above described digitizing process can be thought of as a landmark acquisition process. Thus, according to a preferred embodiment of the present invention, landmark points and/or directions are digitized with respect to the femur **2** and the tibia **4** utilizing the pointer **160** and are stored in the computer **120**. Preferably, an anatomical coordinate system for the femur **2** and the tibia **4** is defined based on at least a portion of the acquired data. The coordinate system can also be defined at least partially using kinematic methods, such as fitting a plane to a trajectory (e.g., fitting the sagittal plane to the flexion/extension trajectory). As discussed in some detail above, possible landmark points include but are not limited to the tibial plateau glenoids, spine, malleoli, the femoral notch, condyles, hip center, bone surface areas, etc. The data acquisition points can be used to determine other information, such as locating a mechanical axis of the tibia **4**.

In a preferred embodiment of the present invention, three dimensional geometrical surface models of the bones are provided by image-free means. Preferably these models are obtained by adjusting a deformable model of the bone to points acquired on the bone surface. Examples of some known methods of carrying out this task can be found in the following references: (1) "Building a complete surface model from sparse data using statistical shape models: application to computer assisted knee surgery" by M. Fleute and S. Lavallee, published in Medical Image Computing And Computer-Assisted Intervention—MICCAI'98, Springer-Verlag LNCS Series, pages 880-887, October 1998; (2) Fleute M, Lavallee S, Julliard R. Incorporating a statistically based shape model into a system for computer-assisted anterior cruciate ligament surgery. Medical Image Analysis. 1999 September; 3(3):209-22. However, other known methods of obtaining geometrical bone models in surgery exist (for example, matching medical image data such as CT, MRI, etc, to points acquired with a pointer or an ultrasound probe). Each of the above listed references is hereby incorporated by reference in its entirety.

In particular, the three dimensional shapes of the involved bones may be provided with image free techniques, such as using bone morphing software which is capable of extrapolating very few range data to obtain a complete surface representation of an anatomical structure (e.g., a bone). The specific details of bone morphing are set forth in the above references but in general, a complete surface model is built from sparse data using statistical shape models. In particular, the model is built from a population of a number of specimen (points), such as femur or tibia points, that are digitized. Data sets are registered together using an elastic registration

method (e.g., the Szeliski and Lavallee method) based on octree-splines. Principal component analysis (PCA) is performed on a field of surface deformation vectors. Fitting this statistical model to a few points in performed by non-linear optimization. Results can thus be presented for both simulated and real data. This method is very flexible and can be applied to any structures for which the shape is stable.

In a preferred embodiment of the invention representations of the femur and tibial bones, or a portion thereof, are displayed on the screen. These models move on the screen in real time based on the motion of tracked femur and tibia. In a preferred embodiment of the invention the system guides the surgeon in manipulating the knee, by using the bone representations as visual aids. Knee manipulations are preferably performed for both "normal" and "abnormal" joint motions. Normal motions can include passive flexion/extension of the knee, with the tibia guided by the medial and lateral femoral condyles. Abnormal joint motions are those indicative of instability in the joint. In other words, the present system preferably is configured to collect data with the pointer **160** in order to perform bone morphing operations or procedures to thus obtain three-dimensional geometrical surface models of the bones. The kinematic data obtained from such motions could also be used to construct the BoneMorphing models, by for example, using the normal direction of a best fit plane to initialize the model. The knee manipulations may also be used to help plan the positions of the implants, for example, to obtain optimal soft tissue balancing around the knee. For example, a femoral component may be positioned such that the gap space between the tibial cut and femoral cut is equal when the knee is in flexion and in extension. Tensors can also be used to balance the knee, for example to apply equivalent forces on each condyle to distract the joint and create joint spaces. The planning of the position of the implants may also be a combination of soft tissue balancing criteria and bone surface, alignment and landmark criteria. Examples of such planning criteria are described in previously referenced United States Patent application No. 20050101966. It is preferable that the algorithm used to plan the position of the implants uses 3D surfaces models of the implants. The 3D surface models of the implants preferably include the outer implant surface and the inner implant surface where the inner implant surface, or at least a portion thereof, can correspond to the surface that needs to be cut out of the bone. This cutting surface can contain planar surfaces or more complex shapes such as curvilinear surfaces, spherical surfaces, or any shape of surface for that matter.

Once the desired position of the implant has been determined, the shape of the cutting surface on the bone can be determined, and the boundary between the cutting surface and the bone surface may be determined. Thus a perimeter around the desired cutting area can be defined and displayed on the computer screen **122**.

The system **100** is particularly suited for joint replacement and resurfacing operations since the computer **120** can be configured for identifying and applying the anatomical coordinate system **170** to at least two bones **2**, **4** of the joint. The anatomical coordinate system **170** can include directions, such as medial-lateral, proximal-distal, anterior-posterior, and so on. The system **100** thus can be configured for identifying landmark points on the surfaces of the bones **2**, **4**. Furthermore, the system **100** can be configured to measure the motion of one bone **2**, **4** in space and to identify the centers of adjacent joints from the measured trajectories. The system **100** can measure the motion of one bone **2**, **4** relative to another for various arcs of joint motion and degrees of joint rotation. In a further aspect, the present invention can provide

a system for determining intra-operatively the three-dimensional shape of the bone surface in the vicinity of the articulating joint and in particular, in the vicinity of the joint surface area to be replaced. Preferably, the three dimensional shapes of the bones are provided with image free techniques.

The computer and robot assisted surgery system 100 according to one embodiment of the present invention is configured to provide a system for guiding joint reconstruction or resurfacing operations on at least a portion of a joint of at least one bone and includes a number of different components that cooperate with one another to perform the intended functions. As shown in FIG. 3, the system 100 can include fixation instrumentation (a fixation assembly) 300, an orienting apparatus 400, a positioning mechanism 500, and guiding instrumentation (guide assembly) 600 for guiding a tool 700, such as a cutting tool, e.g., a saw-blade or milling tool.

FIGS. 4a-7 illustrate one exemplary fixation assembly 300 which is intended to secure the orienting apparatus 400 and the positioning mechanism 500 onto the bone 2 (femur). As will be described in greater detail hereinafter, the orienting apparatus 400 and the positioning mechanism 500 are intended to align and position the guide assembly 600 with respect to the intended implant position in the femur 2. The guide assembly 600 is intended to provide an interface between the positioning mechanism 500 and the tool 700. As will be appreciated below, these system components are constructed to introduce a number of degrees of freedom into the system 100.

The fixation assembly 300 preferably includes a fixation means for rigidly fixing at least a part of the orienting apparatus 400 to the femur 2. For example, the fixation means can be in the form of a number of fixation fasteners that fix the orienting apparatus 400 to the femur 2. Suitable fixation fasteners include but are not limited to Stienman pins, threaded pins, screws, cannulated screws, fixation nails, or other types of fasteners. For ease of simplicity, these various means of fixation will be hereinafter generally referred to as fixation pins 310. The fixation pins 310 are elongated structures and each can include a head portion and typically includes a sharp, pointed distal end 312.

The fixation assembly also includes an anchor element 320 that is fully or partially inserted inside the femur 2. The illustrated anchor element 320 has an elongated body 322 that is at least part hollow and includes a first open end 324 and an opposing second closed end 326. The first open end 324 can include a first locking or locating feature 326, such as a notch, for forming a keyed type coupling with a guide element 330 described below. The illustrated anchor element 320 has a cylindrical body 322 and includes a number of through holes 328 passing therethrough, as well as a having a central bore 325 that is open at the first end 324. More specifically, the through holes 328 are formed through the side of the anchor element 320 between the first and second ends 324, 326. The number of and the size of the through holes 328 are selected so that the through holes 328 accept the fixation pins 310. In other words, the fixation pins 310 are slidably received through the holes 328 in the body 322 so that they can pass completely therethrough into the femur 2. The anchor element 320 can be relatively short so as not to enter substantially into the intramedullary canal in the diaphyseal portion of the femur 2.

A cylindrical body 322 allows the surgeon to control the rotational position of the fixation pins 310 with respect to the bone 2 after the anchor 320 is inserted through the drill hole and into the bone 10. Alternatively, a non-circular cross-sectional shape could be incorporated into at least a portion of the anchor, to block rotations and increase stability. For

example, a star shape could be used near the distal end of the anchor 320 so that rotation can be controlled, while the anchor 320 is partially inserted, and then fixed once it is fully inserted.

Alternatively, a longer anchor 320 that enters the intramedullary canal at least partially could be used to improve fixation stability if needed.

The guide element 330 is configured to be rigidly yet removably attached to the anchor element 320 and can be used to guide the insertion of objects so that it each engages one of the through holes 328 formed in the body 322 of the anchor element 320. For example, the guide element 330 can be used to guide the insertion of the fixation pins 310 or guide wires or the insertion of a bone drill or the like for making a hole in the femur 2, so that these objects engage and pass through the holes 328 formed in the body 322 to therefore be anchored to the bone 2. FIG. 4a illustrates the guide element 330 being removably coupled to the body 322 of the anchor element 320, while FIG. 5 shows these parts inserted into the distal femur. FIG. 6 shows the anchor element 322 inserted into the distal femur with the fixation pins 310 passing therethrough and the guide element 330 being removed.

As best shown in the exploded view of FIG. 7, the guide element 330 includes a base portion or body 332 with an arm 334 extending outwardly therefrom. As best shown in FIG. 4a, when the guide element 330 is mated with the anchor element 320, the base portion 332 is disposed on an outside of the femur 2, while the arm 334 extends across either below or above the bone, in this case below the distal portion of the femur 2, so as to position the arm 334 in proper relationship with the anchor element 320 to permit the anchor element 320 to be inserted into the distal femur 2.

The base portion 332 contains a number of through holes 335 formed therein which receive the fixation pins 310 and more importantly, the holes 335 are substantially collinear with the holes 328 in the body 322 of the anchor element 320 so that when the fixation pins 310 are inserted and passed through the holes 335 of the guide element 330 they exit the body 322 and pass across a space between the two bodies 322, 332 where the femur 2 is present, through fixation holes formed in the femur 2 and then into the holes 328 of the anchor element 320 as shown in the figures. It will be appreciated that the holes 328, 335 are made substantially collinear by fixedly attaching the guide element 330 in a predetermined orientation relative to the anchor element 320. More specifically, when the guide element 330 is coupled to the anchor element 320, the proper alignment between the holes 328, 335 results. The holes 335 are thus substantially parallel to one another. At least a portion of the pins could be threaded. As illustrated in FIG. 4b, the pins 310 could also have a tapered portion 380 somewhere along their length. Thus the pin can have more than one diameter, and any portion can be threaded. The taper in the pins can interface with a corresponding taper in the holes of the anchor element 320, so that when the tapered portion of each pin comes into contact with the anchor, a force is produced that tends to push or pull the anchoring element against the bone for increased stability.

In yet another instance of the invention, anchor element 320 can be constructed to expand inside the bone, for example, when at least one fixation pin 310 is inserted. The expansion mechanism can be realized in a number of ways. For example, the anchor element 320 can have a thin slot (not shown) cut through it (for example, about 1 mm thick), where the slot is coplanar to the axes of the pin holes 380, dividing each of them into two portions, an anterior and posterior portion. The slot can start from one end of the anchor element (for example the distal or proximal end) and can stop just

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before the opposite end, leaving some material at the opposite end to act as a hinge or flexure joint to facilitate the expansion action. The holes **328** in the anchor element can be configured with a diameter smaller than the largest diameter of the pin such that when pin **310** is inserted into hole **328**, the larger pin diameter enters the smaller hole and tends to expand the effective diameter of the anchor element, elastically deforming the flexure joint and prying apart the two inner faces of the slot. In yet another variation of the invention, at least one of the holes can be absent, allowing the complete diameter of the pin to pry apart the anchor element when it enters the slot.

The arm **334** of the guide element **330** has a through opening or bore **337** formed at a distal end thereof such that the bore **337** passes through an underside **338** to a topside **339** of the arm **334**. An axis of the bore **337** intersects axes of the holes **335** since the axis of bore **337** is not parallel to the axes of holes **335**.

It will be understood that the guide piece **332** can include a sliding joint (not shown), such as a “dove tail” or “T” joint, located between the arm **334** and pin holes **335**, with a direction parallel to pin holes **335**. This allows the guide holes to be slid directly up against the bone surface to increase rigidity during drilling or pinning, while maintaining the co-linearity between the guide holes **335** and the anchor holes **328**. In addition, the guide face that touches the bone surface can contain at least one sharp spike to prevent it from sliding on the bone surface during pinning or drilling.

In a preferred embodiment, the robot fixation pins **310** are installed in the femur before the femoral reference marker **142** is attached to the bone. The femoral reference marker **142** can then be attached directly to the robot fixation pins **310**, via a base element **450** that fits and clamps onto the exposed portion of the robot fixation pins (FIG. 3). This minimizes the amount of screws placed in the bone. The femoral reference marker can be attached to the base element via an extending structure **460** having several centimeters in length, so as to ensure the reference marker is visible by the camera and does not interfere with the robot or other instruments during the procedure. The base element has a coupling interface to connect with the robot manual orientation system **400**. In another embodiment, at least one of the manual orientation degrees of freedom **432** is incorporated directly into the base element. At any time during the procedure, the surgeon can check if the fixation pins or reference marker has moved relative to the bone by placing the point probe **160** on a confidence point such as an identifiable point on the bone surface or on another small screw or pin (not shown) placed in the bone.

To couple the guide element **330** to the anchor element **320**, a coupling spacer **340** is provided to mate with and be disposed between the arm **334** and the anchor element **320**. The spacer **340** is a generally hollow member that has a through bore **341** formed therethrough from a first end **343** to a second end **345**.

The arm **334** preferably includes a second locking or locating feature **350** that is complementary to and engages a third locking or locating feature **352** formed at the first end **343** of the spacer **340**. The spacer **340** also includes at the second end **345** a fourth locking or locating feature **354**. In the illustrated embodiment, both the third and fourth locating features **352**, **354** are in the form of a tab or detent or protrusion formed at the respective end and extending outwardly beyond the respective ends of the spacer **340**. The protrusions **352**, **354** extend in opposite directions but along the same axis of the spacer **340**. The protrusion **354** is complementary to the notch **326** so that it can be received therein to couple the second end **345** of the spacer **340** to the anchor element **320**. Similarly, the protrusion **352** is complementary to the slot or opening

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350 formed in the arm **334**. It will be appreciated that when the protrusions **352**, **354** engage the second locating feature **350** (e.g., a longitudinal slot or notch formed in the arm **334**) and notch **326**, respectively, each of the three parts (anchor **320**, guide **330** and spacer **340**) is prevented from rotating independent of the other parts. These locating features thus not only locate each part relative to the other part but they also rotationally lock each part with respect to the other parts.

As best shown in FIG. 7, the guide element **330**, spacer **340** and anchor **320** are coupled to one another by means of a fastener **370**, such as a pin. The pin passes through the bore **337** formed in the arm **334**, then passes through the bore **341** of the spacer **340** and into the bore **325** of the anchor element **320**. Advantageously, the guide element **330**, as well as the spacer **340**, can be made to disassemble from the anchor element **320** so that it can be removed and not interfere with the cut after the fixation pins **310** have been properly inserted into the femur **2**. The entire anchor fixation system defined by the above parts has the advantage of increased rigidity in particularly soft or weak bone, which is often present in patients suffering from osteoarthritis. However, in patients with very hard and strong bones, using fixation pins **310** or screws alone can be enough to obtain a sufficiently rigid connection.

Once the fixation pins **310** have been properly located in the femur **2** to support the other components of the overall system **100**, the orienting apparatus **400** is then attached to the fixation pins **310**. FIG. 3 illustrates one exemplary orienting apparatus **400** according to the present invention. The orienting apparatus **400** is generally formed of two parts, namely a base **450** and a second part that is movably coupled to the base **450** and provides an interface to the positioning mechanism **500** (FIG. 3). The base **450** has a body that attaches to the fixation pins **310** by a number of different means, including providing a clamping mechanism. Such a clamping mechanism can be realized using a slot cut out of the body, where at least a portion of the slot intersects with the two axes of the fixation pins **310**. A clamping screw, can be arranged in-between in-between the two pins such that when the screw is tightened, the body flexes and clamps onto the fixation pins **310**. Slot can be made by wire cutting, for example, and the slot path cut can be made so as to have two areas of flexure in the body such that the clamping action is a parallel one, applying a more or less equally on force on each fixation pin.

FIGS. 8 and 9 illustrate another exemplary orienting apparatus **400** according to the present invention. Again, the orienting apparatus **400** is generally formed of two parts, namely a base **410** and a second part **420** that is movably coupled to the base **410** and provides an interface to the positioning mechanism **500**. The base **410** has a body or sliding joint **412** that attaches to the fixation pins **310** by a number of different means, including providing complementary fastening members, such as threaded screws **414**, associated with the body **412**. These screws **414** can be used to rigidly fix the base **410** of the orienting apparatus **400** onto the pins **310**. The fixation pins **310** are aligned with the screws **414**, which are then tightened to cause the body **412** to be securely and fixedly attached to the fixation pins **310**. As illustrated, the screws **414** run along a length of the base **410**.

The sliding joint described above provides a means of easily separating the fixation assembly **300** from the base **410** or **450**.

In another embodiment, the base **410** or **450** of the orienting apparatus **400** is integral to the fixation assembly **300** and more particularly, to the pin guide **330** and fixation pins **310** such that once the fixation pins **310** are inserted, the base **410** is already fixed upon the femur **2**. This will save considerable

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time and effort during the fixation step of the procedure since the step of fixedly attaching the orienting apparatus 400 to the fixation pins 310 is eliminated.

The second part 420 is movably attached (e.g. pivotally) to the base 410 so as to provide the orienting apparatus 400 with at least one rotational degree of freedom. This rotational degree of freedom rotates in a direction that is generally aligned with the varus/vargus direction of the implant. As is known in the field, the term “varus” refers to an inward direction and the term “valgus” refers to an outward direction and these terms refer to the direction that the distal part of the joint (or bone depending upon the point of reference) points. This degree of freedom can be lockable by means of a fastener, such as a screw, or by means of a quick locking cam mechanism.

Preferably, the orienting apparatus 400 includes another rotational degree of freedom. As illustrated in FIGS. 3, 8, and 9, the orienting apparatus 400 can include a first rotational degree of freedom along axis 430 and a second rotational degree of freedom along axis 432, with one of these rotational degrees of freedom being in the varus/vargus direction and the other being generally aligned with the transverse rotation directions of the implant. This additional rotational degree of freedom can likewise be lockable by means of a fastener (screw) or by means of a quick locking cam mechanism.

As best shown in the cross-sectional view of FIG. 9, the rotatable second part 420 is connected to the base 410 at least along the axis 430 as by means of a first shaft or the like 434 to thereby permit the second part 420 to rotate about the axis 430. The second part 420 includes a body 422 that is rotatably coupled to the first part 434 to permit rotation of the body 422 about the first axis 430. The body 422 of the second part 420 is also preferably rotatably coupled to a second part 436 to permit rotation of the second part 420 about the second axis 432.

Thus, the body 422 has at least two degrees of rotational freedom with respect to the base 410. In this manner, the orienting apparatus 400 (adjustment system) is similar to a universal joint, with two rotational axes arranged perpendicular and intersecting to one another as illustrated in FIGS. 8-9. These two rotational axis can also be non-intersecting as shown in FIG. 3. Here, the varus/valgus rotation axis 432 is along the axis of screw 456, and the internal/external rotation axis 430 is about pin 452. The body 422 of the second part 420 includes a mounting or interface section generally indicated at 440. This section 440 can be in the general form of a mounting plate which is preferably planar in nature as illustrated. As described below, the positioning mechanism 500 is coupled to the orienting apparatus 400 by being mounted to the section 440. The section 440 is formed along one face of the body 422 that faces away from the base 410. In the illustrated embodiment, the section 440 has a pair of spaced, outwardly extending wings or tongues 442 that have openings 444 formed therethrough to receive fasteners or the like to fixedly couple the positioning mechanism 500 to the orienting apparatus 400. In another embodiment, especially when only the fixation pins 310 are used alone, the orienting apparatus 400 can be fixed as indicated in FIGS. 3 and 10, such that rotational axis 432 corresponds to the “varus” rotation.

In one embodiment and as will be appreciated more below, the fixation assembly 300 and the orienting apparatus 400 provide a fixation and adjustment system that secures the robotic components of the present invention to the femur 2 and incorporates a two degree of freedom adjustment mechanism which permits the surgeon to align (e.g., manually) an

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axis associated with the robotic component to the implant profile in both the frontal and transverse (or axial) planes 50, 60 (FIG. 1).

The positioning mechanism 500 is connected to the orienting apparatus 400 and similar to the orienting apparatus, the positioning mechanism 500 is constructed so that it has a rotational degree of freedom. More specifically, the positioning mechanism 500 is constructed so that it includes at least two rotational degrees of freedom that have rotational axes arranged substantially parallel to one another, and substantially orthogonal to the axes 430, 432 of rotation of the orienting apparatus 400. Thus, the rotational axes of the positioning mechanism are substantially parallel to the flexion/extension axis of the implant.

As shown in FIGS. 10-18, the positioning mechanism 500 includes a body 510 that has a first section 512 and a second section 514 spaced therefrom. Each of the first and second sections 512, 514 includes an arm or finger 516, 518, respectively, at distal ends thereof and includes head portions 517, 519 at opposite ends thereof for mating with an actuator as described below. The first section 512 includes a first rotational axis 520 (FIG. 3) of the positioning mechanism 500, while the second section 514 includes a second rotational axis 522 (FIG. 3) of the positioning mechanism 500 which is substantially parallel to the first rotational axis 520. In the illustrated embodiment, the first section 512 and therefore, the first rotational axis 520, is coupled to the orienting apparatus 400, while the second rotational axis 522 is attached to the guide assembly 600, which provides an interface between the positioning mechanism 500 and the tool 700. As previously mentioned, the orienting apparatus 400 and the positioning mechanism 500 are intended to align and position the guide assembly 600 with respect to the intended implant position in the femur 2.

A central section 515 separates the first and second sections 512, 514, such that the first and second rotational axes 520, 522 of the positioning assembly 500 are separated by a distance such that the combined rotation of the first and second rotational axes 520, 522 changes the guide assembly 600 positioning in the sagittal plane 70 (FIG. 1) in one rotational degree of freedom, as well as two translational degrees of freedom. These degrees of freedom correspond substantially to flexion/extension implant rotation, AP implant positioning, and PD implant positioning.

Within each of the first and second sections 512, 514, there is a rotatable element, such as a shaft, that rotates about one of the first and second rotational axes 520, 522, respectively. In other words, the first section 512 has a first rotatable element associated therewith, while the second section 514 has a second rotatable element associated therewith. Each of the first and second rotatable elements is operatively coupled to an actuator or the like that selectively imparts controlled rotation to one of the first and second rotatable elements. At the distal ends of the first and second sections 512, 514, the first and second rotatable elements can be operatively coupled to another member, such as the orienting apparatus 400 or the guide assembly 600, to translate rotation to the members or to rotate the positioning mechanism 500 relative to the member, keeping the cutting guide axis substantially aligned with the axes 522, 520.

The two rotational axes 520, 522 of the positioning mechanism 500 can be actuated manually or the axes 520, 522 can be actuated in an automated manner. The actuation can be caused by any number of different types of mechanisms, including any type of actuation motor, including electromagnetic, piezoelectric, brushless, stepper, pneumatic, etc., or the actuation can be caused by any other known means of actua-

tion. For ease of illustration, the actuation of the rotatable elements is discussed as being caused by an actuator, such as a motor, which is generally indicated at **550** and is associated with one of the rotation axes **520**, **522** of the positioning mechanism **500**. Thus, the positioning mechanism **500** can be discussed as having a pair of actuators **550** for the two rotatable elements in the two sections **512**, **514**. The actuators **550** can be in the form of a single module (FIG. **14**) or motor pack that is operatively coupled, in a detachable manner, to the heads **517**, **519** of the positioning mechanism **500** such that each of the first and second rotatable elements in the two sections **512**, **514** is operatively coupled to one of the actuators **550** (motor or the like). The actuators can thus be in the form of a pack that contains two independently operated motors and is configured to detachably interlock with the two heads **517**, **519** of the positioning mechanism **500**. The body **510** of the positioning mechanism **500** can be thought of as a gear and brake unit that is detachably coupled to the actuator (motor) unit **550**.

In another different embodiment, the motors are directly integrated into the gear unit such that they are in the same housing, as illustrated in FIG. **3**. In particular, the motors can be arranged within the housing **500** so that they lie in between **524** the two axes of rotation **520**, **522**, and are connected to the axes via gears, for example, spur gears (not shown). This makes for a particularly compact unit.

In the automated embodiment, where the two rotatable elements are actuated automatically, the surgeon does not have to align manually by hand both the flexion/extension implant rotation and the AP and PD implant positioning. This results in a savings of time during the position step of the procedure and makes the overall system **100** easy to use for the surgeon. Furthermore, precision gears can be included at each rotational axis **520**, **522** (e.g., at each rotatable element) of the positioning mechanism **500** to increase the guide positioning accuracy. It will therefore be appreciated that upon actuation, one of the rotatable elements is rotated about its respective rotational axis to directly translate a rotational force to the member that is operatively coupled thereto. In the case when the first rotatable element is coupled to the orienting apparatus **400**, the orienting apparatus **400** can be caused to rotate about the first rotational axis **520**, while when the second rotatable element is attached to the guide assembly **600**, the guide assembly **600** and the tool **700** attached thereto can be caused to rotate about the second rotational axis **522**.

The positioning mechanism **500** can also include a brake mechanism **560** as shown in FIG. **10**. The brake mechanism **560** is constructed to prevent the first and second rotatable elements from rotating about rotation axes **520**, **522** as long as the brake is not released. The brake mechanism **560** can be electromechanical or manual and can be spring loaded such that the surgeon must interact with an interface, such as for example, the pressing of a button **562** or turning of a knob to disengage the brake mechanism **560**. In addition, the brake mechanism **560** can be configured so that a single interface button disengages the brake mechanisms from both rotation axes **520**, **522** simultaneously. The brake mechanism **560** can be configured to block rotation at the transmission level of the precision gear reducer inputs so that any small rotational deviations caused by the engaging action of the brake are reduced by the gear reduction ratio at the guide positioning level.

According to one exemplary embodiment, the brake mechanism **560** is in the form of a manual spring-loaded brake that is disposed in between the zero-backlash gear inputs and the motor outputs. In this embodiment, the surgeon

must hold the safety button **562** in order to release the brake and free both gear inputs to rotate.

Using brake mechanism **560** has several advantages for safety and convenience. When using actuators (e.g., motors) to position the guide assembly **600** (e.g., cutting guide), the brake mechanism **560** ensures that (1) the guide assembly **600** maintains its position regardless of the state of the actuators; and (2) the actuators cannot move the guide assembly **600** unexpectedly if the button **562** is not depressed. Additionally, since the actuators **550** can be removably attached to the gear unit of the positioning mechanism **500**, they can be easily replaced during the procedure in case of failure or malfunction. A system that is configured with brake mechanism **560** and removable actuators **550** also has the advantage that the overall weight of the positioning mechanism **550** can be reduced during the cutting stage. Because of the quick-release brake mechanism **560**, the surgeon only needs to mount the motors **550** to the gear interface that can be present in the heads **517**, **519** of the positioning mechanism **500** before making each of the five femoral TKA cuts to align the guide assembly **600** to the cutting plane.

Since the brake mechanism **560** bears the loads applied to the guide assembly **600** during the cutting phase, the motors **550** need only provide enough power to position the cutting guide assembly **600**. The motors **550** can be lower torque motors **550** that provide sufficient torque to lift the cutting guide **600** with the brake released, but not enough force to pose any significant threat. Moreover, the surgeon can overpower the motors **550** and backdrive the system in the case of a controller malfunction. In case of a motor or cable failure in surgery, the actuators **550** are designed as a modular system in which the motors **550** are encapsulated in a separate housing so that they can easily be detached from the gear unit in the positioning mechanism **500** and replaced. Therefore, this configuration allows a hospital to use the motors **550** until the end of their lifespan and then to dispose and replace the motors **550** after failure without having to stop the surgery and dismount the robotic parts. Finally, because of the quick-release brake mechanism **560**, the surgeon only needs to mount the motors **550** to the gear block interface in the positioning mechanism **500** before making each cut to align the guide assembly **600** to the cutting plane, the motor unit and power cable do not need to be connected to the robot during a cutting phase or milling phase when the surgeon is typically standing directly beside the knee. This permits the guide **600** to be very compact and lightweight. This option becomes more important in patients having very poor quality bone where the fixation rigidity could be compromised.

One exemplary guide assembly **600** is shown in FIG. **11** and the modular nature of the system **100** of the present invention permits attachment to the various cutting guide interfaces **600**, such as saw-guides or milling tool guides. FIG. **11** shows an exemplary saw-blade guide **610** being attached to one of the first rotatable element associated with the first section **512** of the positioning mechanism **500**. The illustrated saw-blade guide **610** preferably includes a slot for receiving a saw-blade. The saw-blade guide **610** can include a linear sliding joint in the plane of the cut so that the saw-blade tip can always be slid up to the start of the cut. This permits the saw-blade guide **610** to slide linearly in the direction indicated by the arrow **601**.

The illustrated saw-blade guide **610** includes a guide arm **620** that extends outwardly from the positioning mechanism **500** and is operatively coupled to the first arm (distal end) **516** of the first section **512** such that rotation of the first rotating element about the first rotation axis **520** results in rotation of the attached saw-blade guide **610** and guide arm **620** about the

first axis of rotation **520**. In this way, the guide assembly **600** can be rotated to a desired location during the procedure so as to position the tool **700** which in the case of a saw-blade guide **610** is a saw-blade **700**. By providing slot **622** and the linear movement along the arrow **601**, this has the advantage to position the saw-guide directly up against the femur **2**, minimizing the unsupported distance of the blade between the edge of the saw-guide slot **622** and the femur **2**. This can minimize the cutting errors due to saw blade bending and skiving.

In order to position the saw-blade guide **610** as close as possible to the inner edge of each cut, a specific cutting order can be used. In particular, if the distal cut is made first, then making an anterior chamfer cut before making the anterior cut results in the saw-blade guide **610** being positioned at the start of both the anterior chamfer cut and the anterior cut. Similarly, making the posterior chamfer cut before the posterior cut results in the saw-blade guide **610** being positioned at the start of both the posterior chamfer cut and the posterior cut.

FIGS. **12-13** illustrate the guide assembly **600** in the form of a milling guide **630** that is configured to be attached to the positioning mechanism **500** to guide a milling tool **700** instead of the saw-blade guide **610**. As shown in FIG. **12**, the milling guide **630** is rotatably coupled to the first rotatable element of the second section **514** of the positioning mechanism **500**. The illustrated milling guide **630** includes a base portion **632** that can include a boss or shaft **634** that is operatively attached to the first rotatable element so that rotation of this element causes the base portion **632** and the remaining part of the milling guide **630** to rotate. A pair of guide arms **636** are provided and are integrally attached at first ends **637** to the base portion **632**. The guide arms **636** are spaced apart from one another so that a space **639** is provided between the two guide arms **636**, with the boss **634** being disposed between the two guide arms **636**.

The distal second ends **638** of the guide arms **636** are open ends and preferably a milling tool joint **640** is disposed between the two second ends **638** of the arms **636**. The milling tool joint **640** has a body **641** with one face **642** that is rotatably coupled to one arm **636**, while the other face **646** of the tool guide block **640** is rotatably coupled to the other arm **636**. The body **641** is thus capable of rotating about an axis within the space **639** formed between the two guide arms **636**, as illustrated by the arrow **645** (FIG. **3**), to thereby permit the tool **700** itself to be rotated relative to the milling guide **620**, which itself can be rotated about the first rotation axis **520**. In other words, the milling tool guide **620** for making planar cuts, such as those performed in TKA, can include at least one rotational degree of freedom (indicated by arrow **645** in FIG. **3**) and at least one translational degree of freedom in the cutting plane, indicated by arrow **647** (FIG. **3**). Thus, the joint **640** includes both elements of rotation and translation and therefore, can be thought of as having a rotational degree of freedom and a translational degree of freedom. The translational degree of freedom joint axis can be parallel to the axis of rotation of the milling tool **700**. The axis of the milling tool **700** can intersect at right angles the rotational degree of freedom axis so as to avoid causing a moment about the rotational axis when sliding the milling tool in the translational direction, indicated by arrow **647** (FIG. **3**). The rotational joint can be connected to the milling guide **620** and the translational joint can be connected to the rotational joint so as to realize a very compact form with a large range of motion.

At least one of the two degrees of freedom of the milling guide **620** can be lockable. Preferably, the degree of freedom that is lockable is the translational degree of freedom. This

allows the surgeon to make the cut in sweeping motions using one degree of freedom at a time. These sweeping motions give better and more stable control of the milling tool **700** while making the cut.

The interface between the milling tool attachment piece **710** and the translational joint **640** can be indexed so as to allow the milling tool **700** to be advanced in discrete intervals. As shown in FIGS. **12, 15** and **19**, the milling tool **700** includes a base or body **702**, with the tool attachment piece **710** being in the form of an elongated shaft having a distal tip **712** and extending outwardly from the body **702**. The attachment piece **710** or shaft includes a number of indexing features **720** formed at spaced intervals along a length thereof. For example, the indexing features **720** can be in the form of circumferential notches formed in the attachment piece **710** and spaced apart from one another a predetermined distance. The distance between two consecutive notches **720** can be the same or the distance can be different. Preferably, these intervals are substantially equal to or slightly less than the axial length of the cutting tool **700**. This maximizes cutting efficiency for a given milling cutter and minimizes the number of passes used to make the cut. Preferably, the indexing system is configured so that it can be switched on or off to accommodate surgeon preference or to allow simultaneous two degrees of freedom motion for following complex trajectories, for example, along the perimeter of a cut plane. In one embodiment, each notch **720** is numbered to provide data indicative of how deep the milling tool **700** is in the patient.

It will also be appreciated that both the cutting device and the milling device **700** has at least three markers so that the device is trackable by the position measuring device **110** using the coordinate system **170**. In particular, the milling device **700** has an axis that has a known spatial relationship relative to the markers. Based upon the known spatial relationship between the drill or milling tip and markers, the position of the drill or milling tip is determined.

Preferably, the milling tool guide **620** can include a slot for guiding a saw-blade, permitting the milling tool **700** to be used for some cuts and the saw-blade to be used for the other cuts. This is particularly useful for making the posterior cut which is surrounded by soft tissues. The use of a continuously rotating cutting tool, such as the milling tool **700**, may in some applications be associated with a higher potential risk than with an oscillating saw-blade. The above slot can also be used to attach a rigid body, for example, the planar probe **160** of the system **100**.

FIGS. **19-20** show the milling tool **700** in greater detail. The distal tip **712** of the milling attachment piece **710** contains a fluted bearing **730** for supporting the rotating cutter and for allowing fluid to pass through to irrigate the cutting side. The bearing **730** can be made out of low friction plastic materials and can also be disposable. The use of irrigation fluid helps to reduce the friction. FIG. **20** illustrates a milling irrigation system. Fluid enters through the base **716** of the attachment piece **710**, as indicated by arrow **715**, and travels within an interior bore of the attachment piece **710** before exiting through the fluted bearing **730**, as indicated by arrow **731**, to irrigate the cutting site in the vicinity of the cutting tool **700**. A low profile ball or needle bearing that allows the fluid to pass in between the balls or needles can also be used.

Now referring to FIGS. **16-19** and according to another embodiment, the milling system of the present invention can be configured so as to allow the machining of non-planar cut surfaces. In this configuration, the longitudinal axis of the milling tool **700** is arranged so that it is parallel to the two rotational axes **520, 522** of the positioning mechanism **500** and the translational degree of freedom is used so as to drive

the milling tool **700** along its axis. Here the positioning (motorized) mechanism degrees of freedom can be used to guide the motion of the milling tool **700** along the direction of the cut. The milling tool can be advanced along the cut by for example holding down the control system footswitch. The robot thus only moves the cutting tool whilst the footswitch is pressed and held down. Different footswitches can be used to control movement in different directions along the cut path. Alternatively, a force sensor can be incorporated into the robot and the movement can be controlled as a function of the forces applied by the surgeon. Thus the surgeon can directly control the position of the milling tool and feel the forces on the robot during cutting. Such control systems exist and are known, such as that used by the ACROBOT robotic system. Such systems are described in many publications, including Cobb J, Henckel J, Gomes P, et al, Hands-on robotic unicompartamental knee replacement, *Journal of Bone and Joint Surgery—British Volume*, 2006, Vol: 88, Pages: 188-197, ISSN: 0301-620X, and Jakopc M, Harris S J, Rodriguez y Baena F, et al, The first clinical application of a ‘Hands-On’ robotic knee surgery system, *Computer Aided Surgery*, 2001, Vol: 6, Pages: 329-339, ISSN: 1092-9088, which are hereby referenced in their entirety. Advancement of the milling guide **620** translational degree of freedom allows for the machining of different contours in three dimensions, one plane at a time.

In one embodiment, the translational degree of freedom is also motorized and sculpting of the bone can be accomplished in all three dimensions instead of in successive planes. Additionally, this translational degree of freedom can be arranged at an oblique angle to the other rotational motorized degrees of freedom, so as to improve the kinematics of milling and so that the milling tool does not interfere with the bone surface. The use of inverse kinematics models are known and commonly used in robotics to control the milling path. Alternatively, more flexible control schemes can also be used such as the ACROBOT control scheme referenced above.

In FIG. **16**, a milling device **700** has a curved side cutter **810** (curved profile) is illustrated and can be used to create a cut surface that matches precisely the shape of the implant. For example, this type of curved side cutter **810** is particularly suitable for use in uni-condylar knee arthroplasty. In this application, the motors **550** can be used to guide the trajectory during cutting for milling of complex shapes, such as curves with variable radii. It will be appreciated that the tool guide **620** allows positioning and locking of the milling tool **700** in the medial-lateral direction to center the implant.

Milling cutters with inward curving implants can be used to machine shapes approximating the original shape of the bone surface to minimize the amount of bone being removed. FIG. **17** is a close-up of a section of FIG. **16**.

Alternatively and as shown in FIG. **18**, a curved cutter **820** that only partially corresponds to the inner implant surface can be used. One exemplary curved cutter **820** is a ball-shaped cutter. Here, straight or curved cutting trajectories are machined into successive planes that can be perpendicular to the two motor axes **520**, **522** (FIG. **3**). The surgeon can manually advance and lock the milling device **700** to the next plane after the cut on the previous plane is finished, by using the indexing system (notches **720**) or by using graduated markings on the milling attachment piece **620** (graduated marker system) or the navigation system **100** to advance the cutting tool **700**. The computer system **120** can be used to control the positioning system **500** so as to adjust the milling trajectory as a function of the contour plane level as measure by the navigation system. In this embodiment, the notches **720** can be closer together to obtain a better surface. The bone **2** can be arranged so that the center of gravity is in line with the fixation

assembly **300** so as to minimize the moment acting on the fixation pins **310** due to the weight of the system **100**.

In another embodiment, the system can be used in an end-milling configuration, so that the axis of the milling tool is substantially perpendicular to the cutting surface. The axis of the milling tool can be arranged such that is perpendicular to the axes of rotation **520**, **522**. This could be particularly useful for cutting curvilinear surfaces, such as those commonly used in unicompartamental knee arthroplasty.

In any of the above embodiments the position of the cutting tool with respect to the bone surface can be displayed in real time. In particular the milling tool can be displayed with respect the boundary of the cut, so that the surgeon known where they are cutting with respect to the edge of the bone, and can pay particular attention so as not to exit outside this boundary in certain zones and injure soft tissues. In particular this boundary can be displayed in different colors, for example, to distinguish areas in which the model is more accurate than others. Accuracy can be estimated by the number of points acquired in the region. Known dangerous zones can also be highlighted, for example where vessels or nerves typically are found.

The present system **100** provides a number of advantages. Using at least one of the following: (1) the identified landmark points; (2) the locations of the joints; (3) the relative bone positions; and (4) the three dimensional shapes of the involved bones, the system **100** can determine an optimal implant position relative to the bone coordinate system **170**. The following is merely a list of additional features that can be incorporated into the system **100** according to the present invention: using probe **160** to navigate and check the location of two fixations pins **310** and the anchor element **320** with respect to planned cuts to make sure they do not intersect any cutting surfaces; a femoral rigid body can be installed at the base of the orienting apparatus **400** to avoid having to install additional pins in the bone **2** to fix the rigid body; calibrating the axis of the milling tool **700** and the diameter of its tip; tracking the milling tool **700** with respect to the bone **2** and displaying the milling tool **700** relative to the bone **2** and in particular, relative to the boundaries of the cut; controlling the milling tool speed as a function of the tool position in the bone; providing a soft tissue guide on the milling tool **700**; incorporating an irrigation system in the tool **700** for spraying out of the cutter bearing; and calibration systems for calibrating the location of the robotic member; the angular index values of the motors **550**; and controlling the position of the motors **550** to align the cutting guide to the implant plan. The present system **100** also provides improved visibility by using only one, slender cutting interface for all of the planar cuts in TKA; it provides a system for positioning the saw-blade guide **610** at the start of the posterior and anterior cuts; it provided an indexed milling tool **700** in which depth advancement of the cutting tool (mechanically optionally) permits the efficient machining and decoupling of the freedom; and it provides a passive cutting guide that allows the surgeon to move a milling tool with a combination of at least one rotation and one translation degree of freedom.

The system **100** can also be configured to measure the motion of one bone in space, and to identify the centers of adjacent joints from the measured trajectories. Furthermore, the system **100** can be configured to measure the motion of one bone relative to another for various arcs of joint motion and degrees of joint rotation. An IM bone plug can be made from bioabsorbable materials and can be left in the bone. These bioabsorbable materials can contain antibiotic type materials to prevent infection, particularly in revision sur-

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gery. It can also serve as a cement restrictor to prevent the cement from entering the intramedullary canal.

The following example illustrates the use of the system 100 of the present invention in a typical surgical procedure.

EXAMPLE

Referring to FIG. 21, the robotic cutting guide of the present invention was integrated into the Surgetics Station®, distributed by the present assignee, which is an open platform surgical navigation system that uses image-free BoneMorphing® (deformable statistical) models to reconstruct the three-dimensional shape of the femoral and tibial surface intra-operatively.

The surgical workflow is present in FIG. 21. With reference to FIGS. 2 and 21, first, the T and F rigid bodies 150, 140 are fixed to the tibia 4 and the femur 2, respectively, and the point probe “P” and planar guide probe “G” are calibrated. These rigid bodies and probes each have at least three passive retro-reflective markers that are localized in three-dimensional space by an optical infrared camera.

To access the knee joint, a medial parapatellar approach with a skin incision length of about 9.5 cm, which is approximately two times the length of the patella. The incision is continued down through the anterior joint capsule and patellofemoral ligament. A 2 cm snip in the vastus medialis in the direction of the fibers facilitates the exposure along with resection of the tibial meniscus and cruciate ligaments.

The tibial maleoli are first digitized to compute the ankle center, followed by the tibial plateaus. These data determine the initial attitude of the BoneMorphing model. The tibial surface acquisitions are then made by manipulating the tibia with respect to the femur in flexion, extension and rotation to help bring the various bone areas into the incision. The patella was not reflected by retracted or subluxed laterally. A conventional tibial cutting guide was then navigated and secured to the anterior tibial surface with two pins. The tibial cut was made with an oscillating saw, and the final cut surface was measured with the planar “G” probe.

The femoral acquisition begins with kinematic identification of the hip center without any rigid bodies in the pelvis. The posterior condyles and Whiteside’s line are then digitized followed by the femoral BoneMorphing surface acquisition. Again, the tibia is flexed, extended, and rotated relative to the femur to expose the different femoral surface areas. There is now more space in the knee as the tibial plateau has already been removed; the tibia can be compressed against the femur and the patella can be distracted laterally. A curved probe facilitates acquisition of the posterior femoral areas with the knee in flexion, and the lateral areas with the knee in extension. Once the surface acquisition is complete, ligament gap measurements between the uncut femoral condyles and the tibial cut surface can be performed at various flexion angles to optimize femoral component positioning and sizing. The system then automatically suggests the optimal position and the size of the femoral implant based on the mechanical axis, the bony landmark features extracted from the BoneMorphing model, and the ligament balancing acquisitions. This proposition can then be checked and modified using the tactile display screen of the computer. Once the femoral implant size and position have been validated, the locations of the five cutting planes are stored in the femoral coordinate system.

The robot fixation pins are then installed in the medial femoral condyle using a guide to help keep the pins parallel and separated by the appropriate distance. To assure that the pins do not intersect any of the five cutting planes, each cutting plane location, along with the position and orientation

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of the “P” probe, are displayed in real time on the navigation screen. The insertion site of the medial collateral ligament along with the planned insertion points of the two fixation pins can be marked on the bone surface to facilitate the insertion. The pin insertion area on the medial side of the femur is bounded by the following structures: anterodistally—by the anterior and anterior chamfer cuts; distally—by the distal cutting plane; posteriorly—by the anterior border of the medial collateral ligament when the knee is in full extension; anterosuperiorly—by the posteroinferior border of the vastus medialis muscle when the knee is in flexion. Fixing the robot in this area permitted uninhibited flexion and extension of the knee, and access to all five cuts through the mobile incision.

4 mm diameter, self tapping fixation pins were used without drilling any pilot holes. The bone quality and density of the fresh cadaver specimen we tested was relatively good, resulting in a rigid and very satisfactory fixation. We are planning a study to assess the rigidity of the two pin configuration in severely osteoporotic bone, however, to see whether or not this fixation technique is appropriate for all patients.

The gear unit with the pre-attached mechanical adjustment system and cutting tool guide are then mounted onto the fixation pins. With the calibrated planar probe (“G” rigid body) inserted in the slot of the guide, robot axis is aligned in varus/valgus and internal/external rotation using the numerical values displayed on the navigation screen. Each degree of freedom can be navigated and locked separately for ease-of-use. Once the adjustments are aligned relative to the planned implant profile, the motor unit is attached and the two kinematic axes and motor angles of the robot are calibrated. This is accomplished by pressing the brake release button on the 2 DOF gear unit, and manually rotating the first robot axis through a range of motion of ~90°. Simultaneous measurement of the motor encoder values and of the “G” rigid body locations with respect to the “F” femoral reference frame are made using the motion controller and the optical camera, respectively.

Using a simple inverse kinematic model that considers the geometry of the robot and the mill or saw-guide, and the position of each cutting plane relative to the robot kinematic axes and encoder calibration constants, the system computes which motor command values correspond to each of the five cutting planes. At this point the robot motors are enabled and the guide can be advanced to the first cut by pressing the system foot pedal and the robot brake release button. The footswitch sends a command to the motion controller to initiate motion of the motors, and the controller monitors the encoder values, notifying the surgeon to engage the mechanical brake once the guide is in position. In addition, the planar guide probe can be inserted in the mill or saw-guide slot to verify the guide position before making a cut.

One preferred cutting order is (1) distal, (2) anterior chamfer, (3) anterior, (4) posterior chamfer, (5) posterior. The distal cut was chosen first in our surgical protocol because it allows the surgeon to visually gauge overall varus/valgus and internal/external rotational alignment, as well as distal cutting depth, before making any of the femoral bone cuts. The anterior chamfer cut was made next followed by the anterior cut so that the cutting guide can be positioned directly against the start of the cut for both cuts, which is an improvement over most over conventional 4-in-1 and 5-in-1 types of cutting guides₍₃₎. This becomes more important when using an oscillating saw, as cutting accuracy is known to diminish with extension of the saw-blade beyond the cutting guide. Moreover, making the anterior cuts before the posterior ones could free more space in the joint for making the posterior cut,

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which is more difficult due to the position of the tibia and the delicate soft tissues behind the knee. Although this is one preferred sequence, the cutting order is not rigid and can be changed to suit surgeon preference. This is quickly and easily accomplished by using the forward or back switches on the system foot pedal to cycle through the cutting sequence. After performing a resection, the accuracy of each cut can be verified using the planar probe. These values are stored into the digital surgical report at the end of the surgery.

While exemplary drawings and specific embodiments of the present invention have been described and illustrated, it is to be understood that the scope of the present invention is not to be limited to the particular embodiments discussed. Thus, the embodiments shall be regarded as illustrative rather than restrictive, and it should be understood that variations may be made in those embodiments by workers skilled in the art without departing from the scope of the present invention as set forth in the claims that follow, and equivalents thereof. In addition, the features of the different points set forth below may be combined in various ways in further accordance with the present invention.

What is claimed is:

1. A system for guiding a cutting tool capable of cutting portions of a bone, comprising:

a fixation assembly having a fastener for attaching the system to a side of the bone;

an adjustment mechanism that includes:

a base for fixedly attaching to the fixation assembly, and a mount pivotably attached to the base about a first axis and a second axis transverse to the first axis;

a positioning mechanism that includes:

a first arm having a first rotational axis, wherein the first arm is mounted to and rotatably coupled to the mount, a second arm having a second rotational axis substantially parallel to the first rotational axis,

a motor configured to rotate at least one of the first and second arms about the respective first and second rotational axes, and

a housing, wherein the first arm, the second arm, and the motor are housed within the housing; and

a guide rotatably coupled to the second arm of the positioning mechanism and rotatable relative to the positioning mechanism about the second rotational axis spaced a fixed distance from the first rotational axis at all rotational positions of the positioning mechanism relative to the adjustment mechanism,

wherein actuation of the motor causes the rotation of the at least one of the first and second arms to adjust a position of the guide relative to the adjustment mechanism.

2. The system of claim 1, wherein the fastener comprises an anchor element configured to be fixedly inserted into the bone and at least one fixation pin that is configured to pass through the bone and coupled to the anchor element by being received through a through hole formed therein.

3. The system of claim 2, wherein the anchor element is an elongated substantially hollow member, with the through hole formed in a side thereof, the fixation pin being an elongated member that is received in the through hole.

4. The system of claim 2, wherein the fastener further comprises a second guide that is detachably coupled to the anchor element and includes at least one guide through hole that is axially aligned with the through hole in the anchor element so as to guide the fixation pin through the bone and into the through hole formed in the anchor element, wherein the second guide includes a base that is configured to be disposed outside and along one side of the bone and an arm

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that is detachably coupled to the anchor element, the base including the at least one guide through hole.

5. The system of claim 1, wherein rotation of the positioning mechanism relative to the adjustment mechanism changes the position of the guide in a sagittal plane of the bone.

6. The system of claim 5, wherein the positioning mechanism further includes a gear unit detachably coupled to the motor, and wherein the motor includes a pair of actuators to cause rotation of the first and second arms about respective rotational axes of the positioning mechanism to cause movement of the positioning mechanism relative to the adjustment mechanism and movement of the guide relative to the positioning mechanism.

7. The system of claim 1, wherein the positioning mechanism includes a brake mechanism that prevents rotation of the positioning mechanism relative to the adjustment mechanism upon actuation.

8. The system of claim 7, wherein the brake mechanism comprises a spring-loaded manual brake mechanism with an interface element, the brake mechanism being actuated by manipulation of the interface element.

9. The system of claim 1, wherein the guide comprises a saw-blade guide including a slot for receiving the cutting tool in the form of a saw-blade, wherein the guide includes a linear sliding joint in a plane of the cut so that the saw-blade guide can be slid closer to or further away from the bone.

10. The system of claim 1, wherein the guide comprises a milling guide that is rotatably mounted to the positioning mechanism to guide the cutting tool which is in the form of a milling tool.

11. The system of claim 10, wherein the milling guide is configured for making planar cuts and includes at least one rotational degree of freedom and at least one translational degree of freedom in a cutting plane.

12. The system of claim 11, wherein an axis of the translational degree of freedom is at least substantially parallel to an axis of rotation of the milling tool, wherein an axis of the milling tool intersects at right angles the rotational degree of freedom of the milling guide.

13. The system of claim 10, wherein the milling tool guide includes a slot formed therein for guiding a saw-blade so as to permit the milling tool to be used for some cuts and the saw-blade to be used for making other cuts.

14. The system of claim 10, wherein the milling guide and the milling tool have an indexing system incorporated therein and constructed such that the milling tool is configured to be discretely advanced into the cut after each cutting swing of the cutting tool.

15. The system of claim 14, wherein an interface between a milling tool attachment piece and a translational joint of the milling guide is indexed so as to allow the milling tool to be advanced in discrete intervals, the indexing being in the form of a series of circumferential grooves formed in the outer surface of the milling tool attachment piece.

16. The system of claim 10, wherein the milling guide and the milling tool are configured to permit machining of non-planar cut surfaces.

17. A system for guiding a cutting tool capable of cutting bone comprising:

a fixation assembly having a fastener for attaching the system to a bone;

an adjustment mechanism that includes:

a base removeably coupled to the fixation assembly, and a mount pivotably attached to the base about two rotational degrees of freedom traversing one another;

a positioning mechanism that includes:

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a first arm rotatably coupled to the mount of the adjustment mechanism, the first arm having a first longitudinal rotational axis,

a second arm spaced from the first arm, the second arm having a second longitudinal rotational axis substantially parallel to and spaced a fixed distance from the first longitudinal rotational axis, and

a motor configured to rotate at least one of the first arm and the second arm about the respective first and second longitudinal rotational axes, wherein the first arm, the second arm and the motor are housed within a housing of the positioning mechanism; and

a guide coupled to the second arm of the positioning mechanism about a sliding joint,

wherein actuation of the motor causes the rotation of at least one of the first and second arms to adjust a position of the guide relative to the adjustment mechanism.

18. The system of claim 17, wherein the adjustment mechanism is coupled to the fixation assembly by a sliding joint.

19. The system of claim 17, wherein the fixation assembly includes an anchor element having a through hole for receiving the fastener therethrough.

20. The system of claim 17, wherein the positioning mechanism has a proximal end and a distal end, and wherein the adjustment mechanism and the guide are each rotatably coupled to the proximal end of the positioning mechanism.

21. A system for guiding a cutting tool comprising:

- a fixation assembly having a fastener for attaching the system to bone;
- an adjustment mechanism that includes:
 - a base fixedly attachable to the fixation assembly, and
 - a mount pivotally attached to the base about two rotational degrees of freedom traversing one another;
- a positioning mechanism that includes:
 - a first arm rotatably coupled to the mount and including a first longitudinal rotational axis,
 - a second arm spaced from the first arm and including a second longitudinal axis substantially parallel to and spaced a fixed distance from the first longitudinal rotational axis, and
 - a motor configured to move at least one of the first arm and the second arm about respective first and second longitudinal axes, wherein the first arm, the second arm and the motor are housed within a housing of the positioning mechanism; and
- a guide coupled to the second arm of the positioning mechanism about a pivot joint,

wherein actuation of the motor causes the movement of at least one of the first and second arms to adjust a position of the guide relative to the adjustment mechanism.

22. The system of claim 21, wherein the positioning mechanism has a proximal end and a distal end, and wherein

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the fixation assembly and the guide are each rotatably coupled to the proximal end of the positioning mechanism.

23. The system of claim 21, wherein the fastener comprises an anchor element configured to be fixedly inserted into the bone and at least one fixation pin configured to pass through the bone and coupled to the anchor element by being received through a through hole formed therein.

24. The system of claim 21, wherein the fixation assembly is configured to attach the system to a medial side of the bone.

25. The system of claim 21, wherein the guide includes a slot for receiving the cutting tool in the form of a saw-blade.

26. The system of claim 21, wherein the guide include a pair of spaced apart planar members forming a slot for receiving the cutting tool.

27. The system of claim 21, wherein rotation of the positioning mechanism relative to the fixation assembly changes the position of the guide in a sagittal plane of the bone.

28. The system of claim 17, wherein the fixation assembly is configured to attach the system to a medial side of the bone.

29. The system of claim 17, wherein the fastener comprises a pair of pins or screws.

30. The system of claim 29, wherein the pair of pins or screws directly attaches to the adjustment mechanism.

31. A system for guiding a cutting tool capable of cutting portions of a bone, comprising:

- a fixation assembly comprising a fixation fastener for attaching the system to a side of the bone;
- an adjustment mechanism that includes:
 - a base for fixedly attaching to the fixation assembly, and
 - a mount pivotally attached to the base about two rotational degrees of freedom traversing one another;
- a motorized positioning mechanism that includes:
 - a housing,
 - a first arm rotatably mounted within the housing, wherein the first arm includes a first longitudinal rotational axis and is rotatably coupled to the mount,
 - a second arm rotatably mounted within the housing and spaced a fixed distance from the first arm, wherein the second arm includes a second longitudinal rotational axis substantially parallel to the first longitudinal rotational axis, and
 - a brake mechanism housed within the housing, the brake mechanism comprising a spring loaded brake, a mechanical brake or an electromechanical brake configured to prevent rotation of the first and second arms relative to the housing upon actuation; and
- a guide rotatably coupled to the second arm of the positioning mechanism and rotatable relative to the positioning mechanism about the second longitudinal rotational axis,

wherein actuation of the motorized positioning mechanism adjusts a position of the guide relative to the adjustment mechanism.

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